Quantification of Forces Dissipated Through Bone When Using Rapid Maxillary Expansion

Nicholas Karaiskos, BSc (Hons Biochem), BSc(Dent), DMD

A thesis submitted to the Faculty of Graduate Studies of the University of Manitoba in partial fulfillment of the requirements for the degree of

MASTER OF SCIENCE (ORTHODONTICS)

Department of Preventive Dental Science Division of Orthodontics University of Manitoba, Faculty of Dentistry Winnipeg, Manitoba, Canada

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BY

Nicholas Karaiskos

A Thesis/Practicum submitted to the Faculty of Graduate Studies of The University of

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Of

MASTER OF SCIENCE

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Abstract

Quantification of Forces Dissipated Through Bone When Using Rapid Maxillary

Expansion

AIM: To Quantify the Forces Dissipated Through Bone When Using Rapid Maxillary Expansion

MATERIAL AND METHODS: Stress-strain gauges (Intertechnology, Don Mills, Ontario) were attached to human adult cadavers and bonded to the bone adjacent to the mid-palatal and intermaxillary sutures using the MBond 200, cyanoacrylate adhesive (Intertechnology, Don Mills, Ontario). The gauges were attached to a P3 machine and forces exerted on the craniofacial complex using a modified RME. Values generated were converted to force in gram units.

RESULTS AND DISCUSSION: After complete activation of the modified RPE appliance, maximum values were compiled and compared. The mean maximum force values for the mid-palatal suture was 986.58 grams (± 203.72), while the intermaxillary suture site was 759.99 grams (± 143.77). These forces are all at the level of orthopaedic in nature. Using a paired student t-test, it was found that there was a statistically significant difference in force values between the mid-palatal and intermaxillary sensor sites (p<0.05). No specimens were found to have either the mid-palatal or intermaxillary suture become patent following complete activation. The difference in values could indicate that the force generated by the modified RME becomes dissipated by the hard and soft tissues in the craniofacial complex and that the further away from the RME, the lower the recorded value. This may further support the theory that piezoelectricity mediates orthodontically induced alveolar remodelling by orthopaedic orthodontic appliances in the craniofacial complex.

CONCLUSIONS: Forces generated by RME devices are dissipated through the bone at levels that exceed orthopaedic force range. The further away from the site of force delivery, the lower the recorded values, suggesting dissipation involves many factors such as amounts of hard and soft tissue.

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1.0 INTRODUCTION AND STATEMENT OF THE PROBLEM

Rapid maxillary expanders (RMEs) are widely used orthopaedic appliances in orthodontics. The use of such expanders exerts forces on the teeth and bone that are dissipated throughout the craniofacial complex resulting in anatomical changes involving bone. Although the literature describes the areas to where this force is dissipated, there is lack of knowledge on the quantification of force at the applied areas and its dissipation throughout the craniofacial complex. Because these appliances are widely used, it is critical to have an understanding of these forces so that an optimal and efficient correction in a biological range can be obtained.

The goal of orthopaedics is to produce a more aesthetic and functional change in the shape of the craniofacial skeleton. This is undertaken by exerting controlled and directed mechanical forces in patients manifesting dentofacial deformities and craniofacial anomalies. This force exerts a strain on the sutures of the craniofacial complex resulting in microscopic changes that over time summate to result in macroscopic effects.

Sutural mechanical stresses during mastication are complex because of momentary changes in force direction, muscle function, complex sutural forms, and the irregular shape of craniofacial bones. Understanding this complex interplay of sutural growth could be the key to understanding the mechanism of action of orthopaedic loading. This will provide invaluable knowledge to the literature in the quest to determine the ideal mechanical stimuli that are necessary when using orthopaedic appliances. This ideal, is the minimum mechanical force that results in the maximum desirable skeletal modification in the shortest period of time. It is anticipated that information from this study will provide improved knowledge to assist clinicians using orthopaedics to provide this optimal force.

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2.0 LITERATURE REVIEW

2.1 Embryology, Anatomy and Histology of the Palate and Sutures

2.1.1 Embryology

The palate begins to develop early in week 6, but the process is not completed until the 12^{th} week. The most critical period during palatal development is the end of the 6th week to the beginning of the 9th week. The entire palate develops from two structures – the primary palate (premaxilla) and the secondary palate. The origin of the primary palate is the deep portion of the intermaxillary segment, which arises from the fusion of the two medial nasal prominences (Figure 1) (Persaud and Moore, 2002).

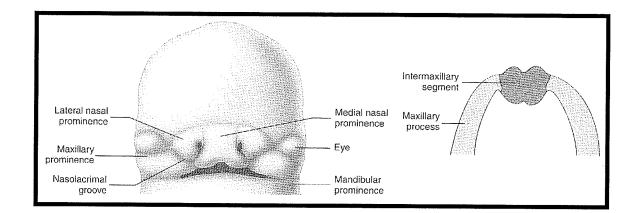
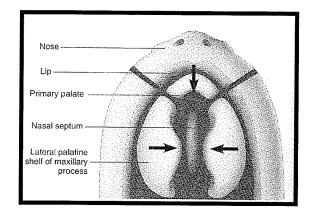
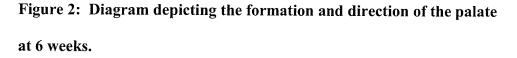


Figure 1: Diagram depicting the formation of the palate from a frontal and coronal view.

The secondary palate gives rise to the hard and soft palate posterior to the incisive foramen. It arises from paired lateral palatine shelves of the maxilla. These shelves are comprised initially of mesenchymal connective tissue and are oriented in a vertical plane with the tongue interposed. Later, the lateral palatine shelves become elongated and the tongue becomes relatively smaller and moves inferiorly. This allows the shelves to become horizontally oriented, to approach one another, and to fuse in the midline. The median palatal raphe is a clinical remnant of fusion between the palatine shelves, and the incisive foramen is present at the junction of the primary palate and the lateral palatine shelves. The lateral palatine shelves also fuse with the primary palate and the nasal septum. Fusion between the nasal septum and palatine processes proceeds in an AP direction beginning in the 9th week (Persaud and Moore, 2002)





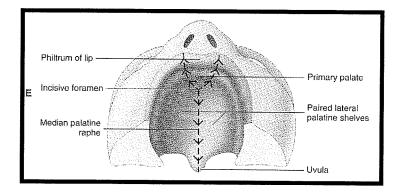


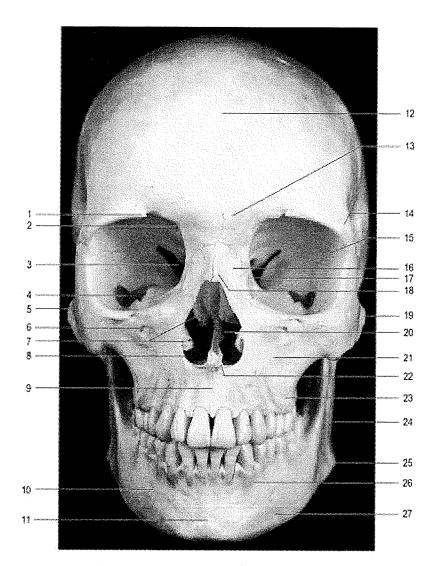
Figure 3: Diagram depicting the formation and direction of the palate at 12 weeks.

The interpremaxillary suture is well-established around the 47th day (Figure 2) of embryo development (primary palate). The first indication of sutural formation of secondary palate, in which the maxillary and palatine parts of the mid-palatal suture form, is at approximately 10¹/₂ weeks of age. A definite intermaxillary suture is established by the 12th week (Figure 3) (Persaud and Moore, 2002).

2.1.2 Anatomy

The maxilla is composed of 2 halves and can be conceptualized as a pyramidal body with 4 sides and 4 processes (Liebgott, 2001). Each maxilla articulates with the following structures (Liebgott, 2001) (Figures 4 and 5):

- 1. The opposite maxilla
- 2. The mandibular teeth (via the maxillary teeth and alveolar process)
- 3. Nasal bone
- 4. Lacrimal bone
- 5. Ethmoid bone
- 6. Palantine bone (via the palatal process)
- 7. Frontal bone (via the frontal process)
- 8. Vomer
- 9. Zygomatic bone (via the zygomatic process, which forms the apex of the pyramid)
- 10. Inferior concha



- Supraorbital notch.
 Frontal notch.
- 3. Superior orbital fissure.
- 4. Inferior orbital fissure.
- 5. Zygomaticofacial foramen.
- 6. Infraorbital foramen.
- 7. Nasal conchae.
- 8. Anterior nasal aperture.
- Intermaxillary suture.
 Mental foramen.

- 11. Mental protuberance.
- 12. Frontal bone.
- 13. Glabella. 14. Zygomatic process of frontal bone.

Figure 4: Front view of skull.

- Greater wing of sphenoid bone.
 Frontal process of maxilia.

- 17. Lacrimal bone.
 18. Nasal bone.
- 19. Zygomatic bone.
 20. Nasal septum.
 21. Body of maxilla.

- Anterior nasal spine.
 Alveolus of maxila (upper jaw).
- 24. Ramus of manditxle.
- Angle of mandible.
 Angle of mandible.
 Alveolus of mandible (lower jaw).
 Body of mandible.

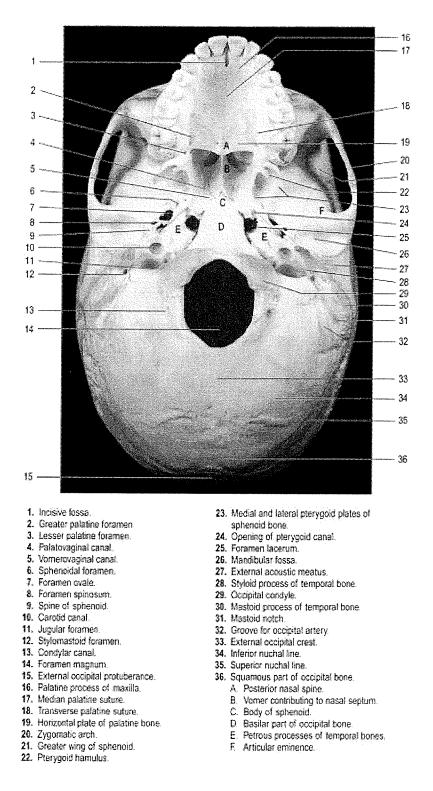


Figure 5: Inferior view of skull.

2.1.3 Histology

It was found by Ten Cate and Freeman in 1977 that the immediate effect of applying tensile force to the palatal suture resulted in small localized tears within the suture, analogous to trauma. The tears then fill with tissue fluids, hemorrhage and an inflammatory cell infiltrate. Granulation tissue replaces the initial hematoma. A considerable number of fibroblasts and mesenchymal stem cells are recruited to the area, and synthesis of type I collagen occurs within the zone where the suture separates. As well, new capillaries form due to the vascular response present. During the active expansion phase, sutural expansion involves injury followed by repair. Regeneration does not occur until the cessation of sutural expansion. There is continued in-growth of new capillaries within this fibrous tissue, and osteoprogenitor cells recruited from the surrounding periosteum begin to deposit osteoid along the collagen fiber network. The response of the suture is one of osteogenesis and fibrillogenesis followed by remodeling (Ten Cate and Freeman, 1977)

Progressive remineralization of the soft callus is next, which is part of the stabilization phase. This phase results in the formation of a hard callus which is composed of immature bone or woven bone. This woven bone undergoes extensive remodelling to restore the normal lamellar architecture (Proffit and Fields, 2003). This returns the bone to its mature level within 3 months (Ekstrom and Henrickson, 1977).

2.2 History and Basis of RME

Over 100 years ago, the foundation of dentofacial orthopaedics was established when Kingsley and Angle discovered that there was a favourable change in patients with dentofacial deformities and malocclusions when an exogenous mechanical stress was applied. The first published work reporting on this procedure appeared in 1860, when E.H. Angell described the rapid expansion of the upper arch to provide space for maxillary canines (Angell, 1860). Since then, a plethora of orthopaedic devices have been established, all having the goal of modifying or altering growth of the craniofacial complex (Proffit and Fields, 2000; Graber and Vanarsdall, 2005). These include headgears, functional appliances and RMEs. The evidence in the literature describing the clinical efficacy of these appliances is exhaustive. However, their exact mechanism of action remains unknown and is a major controversy in the orthodontic literature. It is thought that exogenous forces produced by these appliances result in sutural bone strain that causes a cellular response in growth (Mao, 2002). This bone strain can be measured on the cortical surface over the craniofacial sutures. Similarly, functional appliances result in an alteration of the muscles of mastication producing stress on the zygomatic, sphenoid and temporal bones due to the attachments of the masseter, temporalis and lateral pterygoid muscles which are articulated by various sutures. (Mao, 2002)

Hylander's macaque model and Herring's pig model have been the foundation of our current knowledge of *in vivo* skull loading in mastication. These *in vivo* bone strain experiments mathematically mapped out the strain endured by the craniofacial sutures in the macaque (Hylander, 1986) and pig (Herring 1991; Herring, Teng, Huang, Mucci and

Freeman, 1996) during mastication. They found that the mandibular condyle sustained large mechanical strain during mastication and the circum-orbital region endures little bone strain, despite the large amount of bone mass present (Picq and Hylander, 1989; Ross and Hylander 1996; Herring, 1991; Herring, Teng, Huang, Mucci and Freeman, 1996; Rafferty and Herring, 1999; Rafferty and Herrig, 2000; Ravosa, Vinyard and Hylander, 2000). Also, sutures withstand mechanical stresses without overstressing facial bones (Buckland-Wright, 1978). Work on goat skulls has demonstrated that sutures absorb considerable energy generated by impact mechanical forces suggesting the possibility that sutural cells and the extracellular matrix components may store strain energy (Jaslow, 1990; Jaslow and Biewener, 1995). Indeed, sutures are moveable joints and have been shown to undergo displacement with moderate orthopaedic forces (Kragt, Duterloo and Algra, 1986).

Sutures are complex soft connective tissue articulations only found in the craniofacial bones of the skull. They absorb and transmit forces from mastication or exogenous orthopaedic forces instantaneously. Sutures, along with epiphyseal plates, allow for longitudinal growth of the skull by bone apposition. Sutures are composed of fibrous connective tissue and epiphyseal plates are composed of hyaline cartilage. Sutural growth is induced by small doses of oscillatory strain as little as 600 cycles 10 minutes per day over 12 days. Oscillatory tensile and compressive strain induces anabolic sutural responses and turns on genes and transcription factors that activate cells through mechanotransduction pathways to stimulate growth. Growth therefore, occurs by hereditary and mechanical signals in the same genetic pathway (Mao, 2002).

The above evidence suggests that sutures experience and transmit mechanical stresses resulting in their modification. An extension from this thinking suggests that orthopaedic forces are also absorbed and transmitted by sutures. The minute movement of the sutural cells due to an orthopaedic force is a potential mechanism for them to activate a biological response.

The literature describes stress patterns of craniofacial bones with RME and headgear using dry skulls. It is assumed that the strain patterns in dry skulls are similar to those *in vivo*. Experiments assessing that sutural strain patterns upon *in vivo* headgear loading in *Macaca irus* are substantially similar to sutural strain patterns in the same locations of dry skulls of the same animals obtained after they are sacrificed (Buckland-Wright, 1978; Kannan, 1982). These experiments help validate the results of dry skull studies. Yet it is assumed that strain is less in dry skulls because they are more stiff than skulls *in vivo*.

A dry skull experiment by Oberheim and Mao (2002) demonstrated that the average peak bone strain of the juvenile temporal articular eminence was significantly higher than the adult articular eminence. This was attributed to three factors:

- 1) a steeper articular eminence in adult skulls
- 2) increased distance from the mesiobuccal cusp of the maxillary first molar to the most inferior point on the articular eminence and
- 3) juvenile bone is more flexible than adult bone and is therefore subject to greater deformation and higher bone strain.

This suggests that similar orthopaedic forces (500 grams) could have different biological effects on immature and mature facial skeletons. They further found that contrasting bone strain patterns are present in the zygomatic arch across the zygomaticotemporal suture. There is an anatomical difference of the zygomatic arch as the middle is bent outwards and the ends are bent inwards. It was found that there was a tensile strain on its lateral surface, but compressive on its medial surface. This suggests potentially differential growth responses, bone remodelling and biomechanical effects of the zygomatic arch upon headgear therapy.

In summary, orthopaedic loading on the dentition results in a transmission of force to produce tensile and compressive strain on the facial and cranial sutures that absorb and transmit these forces. Different sutures experience different strain. Sutures absorb these stresses and their bony edges are displaced, either through tension or compression. This results in modulating sutural growth at the cellular level resulting in overall growth modification. Further, different sutures have different responses to force and propagate that force mainly into tensile or compressive strain (Figure 6).

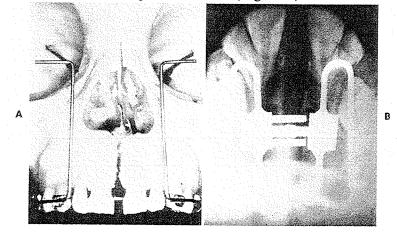


Figure 6: Opening of the mid-palatal suture on a dried skull (A). Radiographic appearance of the opened suture (B).

2.3 Types of Appliances Used for Rapid Maxillary Expansion

There is a wide array of appliances that can be utilized to accomplish rapid maxillary expansion:

- Removable appliances: These appliances provide mid-palatal splitting and are generally effective in the deciduous or early-mixed dentition. The predictability of these appliances is not great, and can be greatly enhanced by patient compliance and sufficient retention (Skieller 1964; Ivanovski 1985; Bishara and Staley, 1987).
- 2) Haas-type banded expander (tissue borne) (Haas 1965, 1980). This appliance is a fixed split acrylic appliance which consists of an expansion screw (spring-loaded or a jackscrew) with acrylic abutting the alveolar ridges. The expansion screw has been shown to deliver 3 to 10 pounds of orthopaedic forces (Issacson, Wood and Ingram, 1964). The appliance is normally attached to the teeth with bands on the first molars and first premolars.
- 3) *Hyrax-type banded expander* (Biederman, 1968). This tooth-borne appliance is a nonspring-loaded jackscrew with heavy wire extensions that are soldered to the palatal aspects of the bands on the first molars and premolars.
- 4) *Minne-banded expander* (Issacson, Wood and Ingram, 1964) is a heavy-caliber coil spring-loaded appliance adapted to bands placed on the first permanent molar.

- 5) *Bonded expander*: This is basically a hybrid of the Haas-type appliance with acrylic covering the occlusal surfaces in a splint fashion. It must be chemically bonded to the maxillary teeth.
- 6) Fan-type rapid maxillary expander: designed in 1996 by Schellino, (Levrini and Filippi, 1999). This expansion appliance incorporates a spider screw named "Ragno" which works asymmetrically and allows "fan opening" of the suture.

2.4 Rapid Maxillary Expansion in Adults

RMEs are one of the most useful appliances used by orthodontists and has been part of the orthodontists armamentarium for over 100 years (Chaconas and Caputo, 1982)

RME's produce high forces that may directly or indirectly affect the ten bones associated with the craniofacial skeleton including the maxilla, mandible, nasal bone, temporomandibular joints and pterygoid plates of the sphenoid bone. Clinicians report difficulty with expansion after the pubertal growth period when the intermaxillary suture is thought to fuse (Bishara and Staley, 1987; Proffit, Fields and Sarver 2007; Işeri, Tekkaya, Oztan and Bilgiç, 1998; Haas, 1980; Hicks, 1978). On the other hand, there is evidence that expansion in young adults is possible (Handelman, Wang, BeGole and Haas, 2000; Stuart and Wiltshire, 2003).

Bone scintigraphy is a technique used to assess the metabolic activity of bone. It's commonly used to detect the vascularity or osteogenesis of bone activity. Baydas and coworkers (2006) performed scintigraphy studies on 17 females age 16.1 to 18.8 years.

Scintography was performed before expansion (T1), at the time the suture was split (T2) and then after the widening period (T3). Significant activity was observed between times T1 to T2 and then there was a remarkable decrease after the suture was opened from T2 to T3. This indicated that in these young female adults, rapid maxillary expansion resulted in not only dental but skeletal effects. This further suggests that RMEs should not be restricted to children. The question that remains to be answered is what is the upper age limit of expansion?

Because histological investigation is not feasible to assess the suture in our patients, an occlusal radiograph is a common technique used in clinical orthodontics to assess if the mid-palatal suture is ossified. A radiological-histological investigation by Wehrbein and Yildizhan analyzed the mid-palatal suture of ten subjects age 18 to 38 years who had recently died. It was found that 50% of the areas in which the suture was determined to be radiologically fused, no histological sutural obliteration was observed. The authors suggest that the term 'fusion' should be avoided when discussing radiological films of sutures. These findings suggest that radiographs should not be utilized to assist in the treatment decision if patients will be able to undergo maxillary expansion. The authors also found that the earliest signs of obliteration were observed in the posterior region of a 21 year old male and one 32 year old male demonstrated no obliteration at all.

In a study of human autopsy material, Melsen and Melsen (1982) described three stages of morphological development of the palatine suture without making reference to the age of the subjects. Their description is of a first stage involving a short, wide-shaped suture with the second stage more tortuous and the third stage an extensive heavy interlocking of the pterygomaxillary connection. They report that the third stage is resistant to vertical and horizontal displacement of the maxilla during rapid palatal expansion

Persson and Thilander (1977) performed a histological examination of autopsy material to investigate the intermaxillary and transverse palatine suture areas of the alveolar arch of twenty-four subjects age 15-35 years. They observed that the palatal sutures may show obliteration in juveniles but a marked degree of closure was rarely found until the third decade. Great variations existed among individuals with respect to the age that the suture began to close. The oldest subject with no signs of ossification was a 27 year-old woman and the earliest ossification was observed in a 15-year-old girl. Variations were also found in different parts of the same suture. Further the closure of the suture progresses more rapidly in the oral versus the nasal part of the palatal vault. The intermaxillary suture was found to close more often in the posterior area versus the anterior. They conclude that there are large inter-individual differences present and that there are other factors other than age that influence the start and advancement of suture closure. They suggest a limit of 5% obliteration of the suture for maxillary expansion to be performed and that most patients under the age of 25 years can undergo the procedure successfully.

Recently, Knaup and coworkers (2004) performed a histomorphometric analysis of autopsy material, from the anterior, median and posterior palate of 22 subjects age 18-63 years. Their goal was to determine the width and degree of obliteration of the mid-palatal

suture between different ages. They found a statistically significant difference in the sutural width between the younger (<25 years) versus the older subjects. Similar to the results of Persson and Thilander, they discovered that the earliest ossifications tended to be observed in the posterior region, confirming a progression of ossification from posterior to anterior. The proportion of ossified tissue in the entire suture (obliteration) was low in all subjects, listed at 13.10%, which was found in a 44-year-old man in the older age group. The median value of the ossification was 0% in the younger age group and 3.11% in the group \geq 26 years and this difference was found to be statistically significant. The earliest ossification was a 54-year-old man.

A very interesting finding of this study was that ossification values were low in all subjects. No sutural region demonstrated more than 15% obliteration. Ossification values were not notably higher for elderly subjects. They suggest that this demonstrated that the bone bridges occurring sporadically within the suture are of no therapeutic significance during the first two decades and orthodontists should be fearful in performing rapid palatal expansion in patients beyond the third decade of life. They did not find bone remodelling or ossification activity lateral to the suture in subjects in the third or fourth decade. Based on Persson and Thilander's suggestion that maxillary expansion is possible with less than 5% obliteration, 77.3% of subjects over the age of 25 would qualify for expansion.

Clinically however, expansion is generally not considered in patients over 25 years due to other maxillary sutures and the age based rigidity of the maxillary bone that are thought to cause resistance to osseous transverse expansion (Isaacson and Ingram, 1964; Kokich, 1976; Melsen 1975; Wertz, 1970). Although the mid-palatal suture may break, there is resistance at the pterygomaxillary interface from the pterygoid plates of the sphenoid bones, which have a tendency to bend laterally and prevent the posterior area of the suture from opening (Wertz, 1970; Chaconas and Caputo, 1982; Jafari, Shetty and Kumar 2003).

In their finite element analysis study, Jafari, Shetty and Kumar (2003) indicates that the pterygoid plates are bent more than 2mm during rapid palatal expansion. Melsen and Melsen (1982) indicated that one cannot count on a spontaneous opening of the pterygomaxillary connection during a rapid palatal expansion due to its extensive interlocking. The stress from rapid maxillary expansion is transmitted to the cranial base only if a fixed pterygomaxillary connection is present and if spontaneous opening does not occur. Protecting the cranial base is therefore important as the elasticity of the bone structures decreases, especially the pterygoid plates of the sphenoid bone. During surgically assisted rapid palatal expansion, there should be a surgical severance of the pterygomaxillary connection (Matteini and Mommaerts, 2001; Holberg and Rudzki-Janson, 2006)

In a finite element analysis of the human cranial base by Holberg and Rudzki-Janson (2006), only moderate stresses were observed in the cranial base of children and

adolescents during rapid palatal expansion suggesting that serious complications are unlikely. In the adult cranial base, due to its reduced elasticity, a considerable amount of stress was present when the pterygoid plates were slightly bent. This stress was particularly evident in the area of the foramen rotundum, the foramen ovale, foramen lacerum and the superior orbital fissure. This suggests that microfractures with injuries to the nervous and vascular structures may occur. Because of the reduced elasticity of the bony structures, considerable stress already occur on light bending of the pterygoid process, especially in the area of the foramen rotundum, the foramen ovale, the carotid sulcus, the optic foramen and the superior orbital fissure, all of which might lead to microfractures with injury of nervous and vascular structures. They suggest that clinicians should be mindful in monitoring the patients' bone elasticity during rapid palatal expansion and that protective measures should be placed in patients with decreased bone elasticity, such as decreasing activations or surgically severing the pterygomaxillary connection.

2.5 Craniofacial Forces from Rapid Maxillary Expansion

The goal of rapid maxillary expansion is to produce a force to displace the palatal suture and expand the palate by forcing the halves laterally, with minimal tooth movement on tipping. This results in heavy forces directed to the maxilla and adjacent skeletal structures. Indeed, patients report pressure sensations at various craniofacial areas during RME, especially the areas articulating the maxilla such as the eyes and the nasal areas (Zimring and Isaacson, 1965; Chaconas and Caputo, 1982). Histological studies of animals where RME was employed also demonstrated signs of increased cellular activity

at various craniofacial sutures. Histological studies have also demonstrated increased cellular activity at the nasal, maxillary-zygomatic and zygomaticotemporal sutures (Starnbach, Bayne, Cleall and Subtelny 1966). The nasal suture demonstrated the most activity. This has been confirmed by other histological studies (Gardner and Kronman, 1971; Starnbach and Cleall, 1964; Storey, 1973; Ten Cate, Freeman and Dickinson, 1977)

Isaacson and coworkers (1964) used strain gauges cemented to RMEs in patients and found that a single activation of the expansion screw of 0.2mm (one quarter revolution) produced approximately 1.3-4.5 kg (3-10 pounds) of force from a single activation. The measured forces were horizontal, vertical and a combination of the two. The force decayed rapidly initially and then continued to slowly decrease. Isaacson found that the resistance of the expansion was not from the mid-palatal suture but from the bones that articulated the maxilla because there was not a significant change in the force when the sutures opened. He found that a smaller force was required for younger patients versus older patients due to less resistance to expansion of the palate. Isaacson did not discuss the magnitude or the nature of changes which occur as activation continues.

Zimring and Isaacson (1965) did a similar study on four patients. They determined that it was the facial skeleton that was the main resistance to expansion. The maximum loads on patients ranged from 7.5-15.7 kg (16.6 to 34.8 pounds) of force during treatment and these forces gradually dissipated during the six week retention period. They reported

forces in other areas such as the nose and beneath the eyes. They concluded that the magnitude and type of forces at these areas are not known.

Haas (1961) sacrificed pigs that had rapid maxillary expansion and found bending in the alveolus and lowering of the palatal vault. By using the data obtained from this pig study, he conducted expansion on human subjects. These subjects noted pressure in the alveolus, palatal vault and the articulations of the maxilla including the frontal, nasal and zygomaticomaxillary suture was recorded. Haas also reported some pressure at the zygomaticotemporal suture in his findings as well. Although these measurements were purely subjective in nature from the subjects, they aided in better understanding the dissipation of these forces.

Investigators have also conducted histological evaluations. Starnbach, Bayne, Cleall and Subtelny (1966) placed RME's on four rhesus monkeys and sacrificed each at different stages of treatment and retention. Histological analysis demonstrated disorganized periodontal fibres with a wider periodontal membrane on the palatal side. There was resorption of alveolar bone on the pressure surface. This was less evident in the animal that had been in retention. There was a predominance of lateral bodily movement over rotational movement. They were able to show greater cellular activity at the nasal, zygomaticomaxillary and zygomaticotemporal suture areas. The most activity was found at the nasal suture and least at the zygomaticotemporal suture.

Gardner and Kronman (1971) also did rapid palatal expansion in six rhesus monkeys and showed distortions at the lambdoid and parietal sutures and the sphenooccipital synchondrosis, by utilizing ultraviolet light. These sutures were split up to 1.5mm at some points, and on one skull the entire parietal bone was elevated above the calvarium. The spheno-occipital synchondrosis was also opened in all experimental subjects and in one animal, the rapid palatal suture expansion led to an opening of more than 1 mm. Histologically, growth or remodelling was evident in bones surrounding the mid-palatine suture such as the infratemporal region of the maxilla, greater wing of the sphenoid, zygomatic arch, pterygoid plates and hamular process.

Storey (1973) showed that the expansion is greater at the alveolar crest compared to the palatal vault. His study involved placing helical torsion springs on the upper lateral incisors of rabbits. Also, the maxillary bones swing laterally with a centre of rotation near the frontonasal suture.

In a study at the University of Manitoba, Murray and Cleall (1971), it was shown that the actual opening of the suture occurred during the fourth to seventh day of expansion in monkeys. It was observed that opening the suture involved a series of distinct stages. There was first an adaptation of the sutural connective tissue to heavy forces, then a proliferation of connective tissue and heavy resorption. This allowed a physical separation of the bony processes. There was then a heavy deposition of bone to maintain the expansion. Furthermore, they found that during the initial stages of expansion, tipping was observed in the buccal dentition, but after 14 days, bodily movement was occurring.

A clinical study by Wertz and Dreskin (1977) on 56 patients aged 8 to 29 years and having undergone expansion therapy with a variety of fixed expansion screw appliances, showed that opening of the palatal suture resulted in the displacement of the maxilla downward and usually forward. This confirmed the work by Gardner and Kronman (1971) who contended that the opening of the spheno-occipital synchondrosis was the reason for the anterior movement of the maxilla. They also showed that older patients had lost the width and younger patients did not have relapse. The older patients had more rigid skeletal components and had little orthopaedic change.

In a study in which metallic markers were placed bilaterally in the maxilla of five patients with bilateral posterior crossbite, age 10-15 years, Hicks (1978) found that a continuous 0.9 kg (2 pound) load was able to separate the two maxillary segments over a 1-3 week time period.

In a study of 32 patients who underwent rapid maxillary expansion, Timms (1980) demonstrated that the palatine bones separated as well as the maxilla and that the pterygoid processes of the sphenoid bone splayed outward. He noted that in subjects undergoing rapid maxillary expansion, the effect is greatest in the dentoalveolar region while it lessens as you move away and as the stress eases.

In a photoelastic study of the human skull, Chocanos and Caputo (1982) measured stresses using RME of the Haas, Minne-expander, Hyrax, and quad helix types. Each of

the appliances produced different stresses transmitted through the bones of the craniofacial complex and effects on the various sutures. This was a result of their having a different range of load-activation characteristics. Fixed appliances produced stress that was concentrated in the anterior region of the palate that progressed posteriorly toward the palatine bone. The Haas, Minne-expander, and Hyrax appliances resulted in stresses that were in the orthopedic range. The stress was concentrated in the anterior region of the palate and progressed to the posterior and radiated to areas superiorly along the perpendicular plates of the palatine bone deeper to anatomic structures such as the lacrimal, nasal, and malar bones, the pterygoid plates of the sphenoid, the zygomatic process and the medial wall of the orbit. Interestingly, increased activation decreased activation, the palate began to separate. The appliance was found to primarily affect posterior teeth. The quad helix appliance was found to produce less than the orthopaedic range of force and was a less effective appliance unless it was used in the very young patient in whom the sutures are patent.

Jafari, Shetty and Kumar (2003) analyzed stress distribution using 3-D finite element analysis on a young dry skull that received rapid maxillary expansion. He found that maximum lateral displacement was 5.313mm at the region of upper central incisors and there was a marked lateral displacement at the inferior aspect of the pterygoid plates. The pterygoid plates approximating the cranial base were minimally displaced. Midline structures experienced a downward displacement with ANS and A point moving down. The expansive forces were found to be distributed throughout the craniofacial skeleton.

Objective #1: To quantify the force levels generated at the mid-palatal suture during activation of the RME appliance.

- *Null Hypothesis #1:* There are no measurable force levels detectable at the midpalatal suture after activation of the RME.
- *Null Hypothesis #2:* The force levels generated at the mid-palatal suture are not orthopaedic in nature (500 grams/16 oz or higher).
- *Null Hypothesis #3:* The maximum force levels generated at the mid-palatal suture do not exhibit statistically significant differences between cadavers.

Objective #2: To quantify the force levels generated at the intermaxillary suture during activation of the RME appliance.

- *Null Hypothesis #4:* There are no measurable force levels detectable at the intermaxillary suture after activation of the RME.
- *Null Hypothesis #5:* The force levels generated at the intermaxillary suture are not orthopaedic in nature (500 grams/16 oz or higher).
- *Null Hypothesis* #6: The maximum force levels generated at the intermaxillary suture do not exhibit statistically significant differences between cadavers.

Objective #3: To determine if the mid-palatal suture remains fused or separates following activation of the RME appliance.

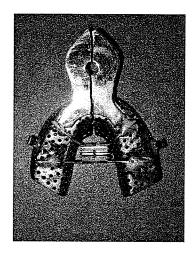
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Null Hypothesis #7: The mid-palatal suture will not break following activation of the RME appliance due to the advanced age of the specimens.

4.0 METHODOLOGY

4.1 Fabrication of a Universal RME Appliance

A stock alginate tray (Ortho Organizers, U.S.A.) that was both perforated and possessed a rim-lock edge was used in an effort to increase the retentive capabilities of the tray. The tray was then modified by cutting it into 2 equal halves and joined in the center by a jack-screw (Forestadent, Pforzheim, Germany) soldered to each half in an anterior and posterior contact point. This jack-screw was capable of expanding a maximum of 12mm in total (Figure 7).





4.2 Sample Selection

Permission was obtained by Dr. Thomas Klonisch of the Faculty of Medicine to perform this study. Human cadavers were selected from those available in the Gross Anatomy Laboratory at the University of Manitoba, Faculty of Medicine. Ethics approval was not necessary as these cadavers were already given the designation for research purposes. Cadavers were chosen that had at least molars and premolars present to allow for better, natural retention of the fabricated RME appliance. The following cadavers were chosen for the study:

Specimen #24009 Male 74 years old.

Specimen #24021 Female 79 years old.

Specimen #23002 Male 68 years old.

Specimen #23011 Female 71 years old.

4.3 Dissection for Sensor Placement

Careful dissection of the cadaver was performed in the palatal and intermaxillary area. In the palatal area, a surgical scalpel was used to place an incision through the keratinized gingival tissue of the palate. This incision followed the line of the teeth (if present) and/or the residual alveolar ridge from the posterior aspect of the second molar to the midline. Next a flap was raised using a periosteal elevator (Hu-Freidy, Chicago, Illinois) to expose bone. The gingival tissue was then removed and discarded in accordance to the rules and regulations governing cadavers at the University of Manitoba. The complete bony palate was now exposed and ready to receive a rosette strain gauge sensor.

For the intermaxillary area, a surgical scalpel was used to cut the gingival tissue in the maxillary anterior area. This incision followed the line of the maxillary anterior teeth (if present) and/or the residual alveolar ridge from the area of the first premolar to the

midline. Next a flap was raised using a periosteal elevator to expose the bone. This flap of tissue was then kept away from the rosette strain gauge site using a retraction fork. Half of the maxillary bone was now exposed and ready to receive a rosette strain gauge sensor.

4.4 Sensor Placement

Once the bone was exposed in either the palatal or intermaxillary sites, it was then cleaned thoroughly with guaze dipped in a 99.9% pure ethanol solution for 5 minutes. Next, dry guaze was used to remove any and all moisture from the respective areas for another 5 minutes. A rosette strain gauge sensor equipped with 6, 10 foot leads (catalogue number C2A-06-062LR-350 (Intertechnologies), Figure 8) was then cemented to the dried bone using MBond200 (Intertechnologies), a cyanoacrylate bonding adhesive (Figure 9). Firstly, MBond 200 catalyst (98% 2-Propanol, 2% n-Phenyldiethanolamine) was brushed onto the back of the sensor and allowed to dry for 10 seconds. Secondly, the MBond 200 cyanoacrylate adhesive was placed on the back of the sensor. With firm finger pressure, the sensor was placed in position and held for 1 minute to allow the adhesive to dry and ultimately bond to the bone.

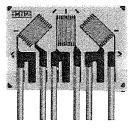
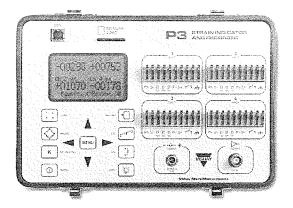


Figure 8: A rosette strain gauge sensor equipped with 6, 10 foot leads (catalogue number C2A-06-062LR-350 (Intertechnologies))



Figure 9: M-Bond 200 (Intertechnologies)

For the palatal suture, the sensor was placed 2mm to the right of the mid-palatal suture and midway between the anterior segment and the junction of the palatal process of the maxillary bone/palatine bone. The orientation of the sensor was such that the leads faced posteriorly or towards the cadaver's throat. For the intermaxillary suture, the sensor was placed 2mm to the right of the intermaxillary suture and 5mm gingival to the highest point of bone from the tooth or residual alveolar ridge. The orientation of the sensor was such that the leads faced inferiorly or towards the cadaver's throat. All leads were then connected to the P3 measuring device (Intertechnology, Toronto, Ontario, Figure 10) such that the first 2 leads were connected to Channel 1, the middle 2 leads were connected to Channel 2, and the last 2 leads were connected to Channel 3.



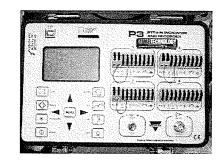


Figure 10: P3 Strain gauge recording device (Intertechnologies)

Once attached to the P3, an ohm meter (Canadian Tire, Toronto, Ontario, Figure 11) was used to ensure that all channels were grounded and stable. If any channels produced readings that were different from the others, this meant that the sensor was not stable and needed to be removed. A stable reading was one where the indicator bar remained stationary in the same range for all channels 1 through 3.



Figure 11: Ohm Meter (Canadian Tire)

Once confirmation of proper placement and functionality (through the ohm meter test) of the sensor was confirmed, the RME appliance was placed.

4.5 Placement and Activation of the RME Appliance and Recording of Strain Values

Kerr brown dental compound (GAC Dentsply, USA) was placed in a water bath and heated to 60 °C. Once this temperature was reached, the compound material was placed and moulded into the modified RME device. The RME was immediately and carefully placed into the oral cavity of the cadaver, seated fully and held into place for 10 minutes to allow for the compound material to cool and harden. Once cooled, the P3 recording device was activated to record changes in the sensor at every second. The RME device was continually activated or turned every 5-10 seconds with use of a special key until it could not be turned any further, for a total of 48 turns or 12 mm. Once the final turn was completed, the P3 was kept in the record mode for another 60 seconds. Results were stored directly on the P3 device on a SD memory card and accessed via personal computer into a Microsoft Excel file (Microsoft Corp., Redmond WA) for analysis.

4.6 Organization of Data and Statistical Analysis

All measurements obtained from the P3 were placed in table form corresponding to the respective channels, namely 1, 2, and 3. Data was then put through a complex mathematical macro developed by Intertechnology Canada to convert the µstrain value and incorporate the multi-directional axes of the rosette strain gauge into a useable format, namely force in grams. Data was analyzed using SPSS Version 15.0 statistical

software (2007 SPSS Institute Inc., Chicago, IL). A two-tailed, paired Student t-test was used to compare the maximum and minimum force values at the different sites for statistical significance between sites and cadavers. A paired t-test is used when each data point in one group corresponds to a matching data point in the other group. The paired t-test is used to investigate the relationship between two groups where there is a meaningful one-to-one correspondence between the data points in one group and those in the other, e.g. a variable measured at the same time points under experimental and control conditions. Two-tailed tests are used where there is no basis to assume that there may be a significant difference between the groups (Hassard, 1991).

5.0 RESULTS

5.1 Cadaver 1 Results

Cadaver 1 yielded the results shown in Figure 12. At first glance it can be observed that there are generally 4 distinct patterns present for each site. For the palatal sensor site, the first phase can be seen as a gradual increase in force values between 0 and 200 seconds. Between 200 and 600 seconds, there is a logarithmic increase in force values with a corresponding levelling-off between 600 and 815 seconds. The final phase shows a slight decline from the initial levelling-off between 815 seconds and the final reading of about 1050 seconds. The intermaxillary sensor site also showed a similar trend, however at different time intervals when compared to the palatal suture site. The first phase is comparable and occurs between 0 and 200 seconds. The second phase, or the logarithmic increase in force values occurred for a shorter overall period between 200 and 450 seconds. The third phase, or the levelling-off portion of the graph occurred between 450 and 750 seconds. The final or fourth phase was observed between 750 and the final reading of about 1050 seconds. The display of a spike in the graph occurred at each activation followed by a period of gradual relaxation and corresponding drop in the force value over time. These spikes were as high as 150 grams of force. The mid-palatal sensor yielded higher force values versus the intermaxillary sensor. According to Table 1, one can view the maximum and minimum values for both sensor sites.

	Mid-palatal	Intermaxillary	Difference
Minimum	319.18	111.58	207.60
Maximum	980.27	862.89	165.38

Table 1:	Maximum	and minimum	force values	(grams) for cadaver 1
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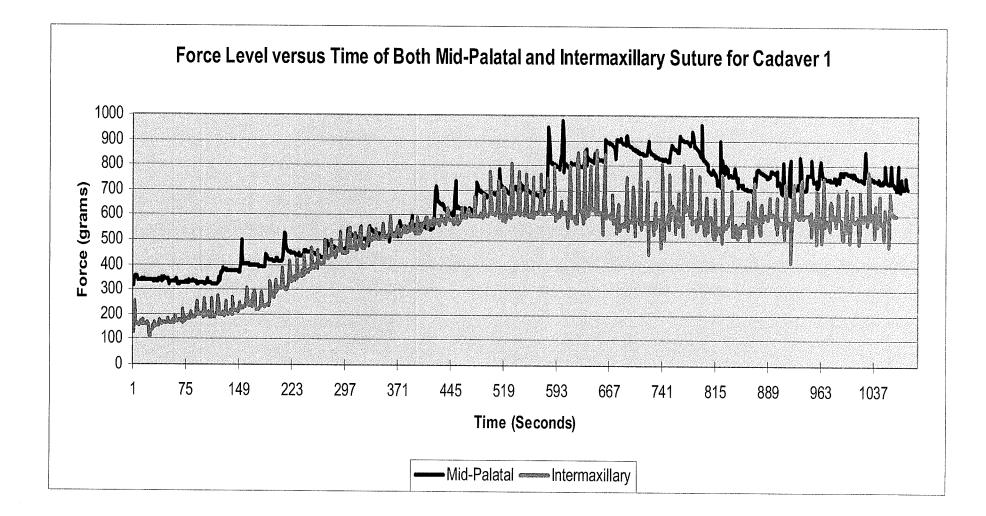


Figure 12: Force level (grams) versus time (seconds) of both mid-palatal and intermaxillary suture for cadaver 1

5.2 Cadaver 2 Results

Cadaver 2 yielded the results shown in Figure 13. This cadaver displayed results that were similar to Cadaver 1. Again, 4 distinct patterns were present for each site. For the palatal sensor site, the first phase can be seen as a gradual increase in force values between 0 and 50 seconds. Between 50 and 175 seconds, there is a logarithmic increase in force values with a corresponding levelling-off between 175 and 275 seconds. The final phase shows a slight decline from the initial levelling-off between 275 seconds and the final reading of about 500 seconds. The intermaxillary sensor site also showed a similar trend, again at different time intervals when compared to the palatal suture site. The first phase occurs between 0 and 50 seconds. The second phase, or the logarithmic increase in force values occurred for a shorter overall period between 50 and 150 seconds. The third phase, or the levelling-off portion of the graph occurred between 150 and 350 seconds. The final or fourth phase was observed between 350 and the final reading of about 500 seconds. Between 300 and 350 seconds, the plateau reached similar levels but here the intermaxillary suture produced higher spikes. The same spikes in the level of force generated were observed at each activation followed by a period of gradual relaxation and corresponding drop in the force value over time. What is notably different in this cadaver is the level of spikes observed with each RME activation. Some spikes yielded increases of almost 300 grams. The mid-palatal sensor yielded higher force values versus the intermaxillary sensor. Table 2 describes the maximum and minimum values for the both sensor sites.

	Mid-Palatal	Intermaxillary	Difference
Minimum	461.36	357.22	104.14
Maximum	1152.42	835.84	316.58

Table 2:	Maximum	and	minimum	force values	(grams)	for cadaver 2
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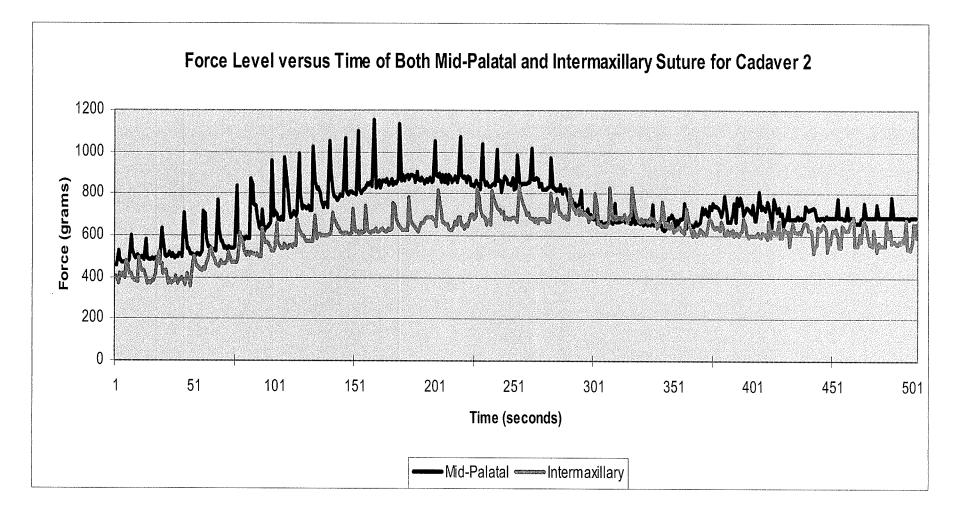


Figure 13: Force level (grams) versus time (seconds) of both mid-palatal and intermaxillary suture for cadaver 2

5.3 Cadaver 3 Results

Cadaver 3 yielded the results shown in Figure 14. This cadaver again displayed results that were similar to the previous cadavers. Again, 4 distinct patterns were present for each site, however a different pattern emerged for the intermaxillary sensor site. For the palatal sensor site, the first phase can be seen as a gradual increase in force values between 0 and 70 seconds. Between 70 and 200 seconds, there is a logarithmic increase in force values with a corresponding levelling-off between 200 and 300 seconds. The final phase shows a slight decline from the initial levelling-off between 300 seconds and the final reading of about 550 seconds. The intermaxillary sensor site also showed a similar trend, again at different time intervals when compared to the palatal suture site. The first phase occurs between 0 and 140 seconds. The second phase, or the logarithmic increase in force values occurred over a longer overall period between 140 and 300 seconds. The third phase, or the levelling-off portion of the graph occurred between 300 and 450 seconds. A sudden drop can then be seen at approximately 451 seconds, followed by the final or fourth phase was observed between 451 and the final reading of about 550 seconds. The same spikes in the level of force generated were observed at each activation followed by a period of gradual relaxation and corresponding drop in the force value over time. The level of increase in these spikes ranged from approximately 200 grams for the mid-palatal sensor site and 50 grams for the intermaxillary sensor site. The mid-palatal sensor yielded higher force values versus the intermaxillary sensor. At about 320 seconds, similar force levels were attained at both sites. According to Table 3, one can view the maximum and minimum values for the both sensor sites.

	Mid-Palatal	Intermaxillary	Difference
Minimum	361.46	199.55	161.91
Maximum	1112.05	792.49	319.56

 Table 3: Maximum and minimum force values (grams) for cadaver 3

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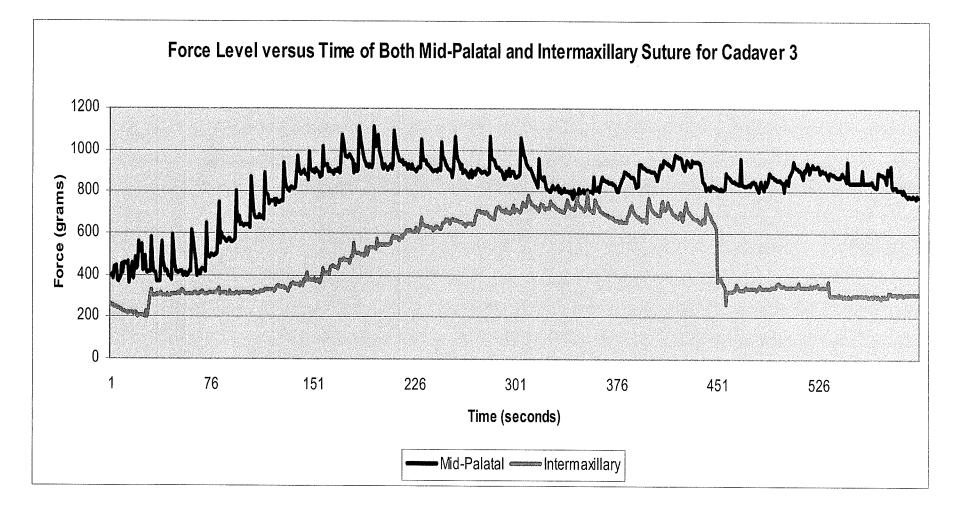


Figure 14: Force level (grams) versus time (seconds) of both mid-palatal and intermaxillary suture for cadaver 3

5.4 Cadaver 4 Results

Cadaver 4 yielded the results shown in Figure 15. This cadaver again displayed a distinct pattern different from the other cadavers, but with generally the same phases. For the palatal sensor site, the first and second phase appear to blend into one between 0 and 135 seconds. Instead of a steady or logarithmic increase in force values, there are spikes and dips not seen before with the other cadavers. Then between 135 and 250 seconds, there is a levelling-off of force values. The final phase shows a slight decline from the initial levelling-off between 250 seconds and the final reading of about 350 seconds. The intermaxillary sensor site displayed the generic pattern we have seen in the other cadavers with the first phase occurring between 0 and 100 seconds. The second phase, or the logarithmic increase in force values occurred over a short period between 100 and 125 seconds. The third phase, or the levelling-off portion of the graph occurred between 125 and 250 seconds, however in this portion, there were not as many spikes present as was customarily seen on the other cadavers. The final or fourth phase was observed between 251 and the final reading of about 300 seconds. The same spikes in the level of force generated were observed at each activation followed by a period of gradual relaxation and corresponding drop in the force value over time. The level of increase in these spikes ranged from approximately 100 grams for the mid-palatal sensor site and 50 grams for the intermaxillary sensor site. The mid-palatal sensor yielded higher force values versus the intermaxillary sensor. At ± 50 seconds, ± 110 and ± 251 seconds, similar force levels were displayed by both sites. According to Table 4, one can view the maximum and minimum values for the both sensor sites.

	Mid-Palatal	Intermaxillary	Difference
Minimum	319.44	312.63	6.81
Maximum	701.59	548.77	152.82

 Table 4: Maximum and minimum force values (grams) for cadaver 4

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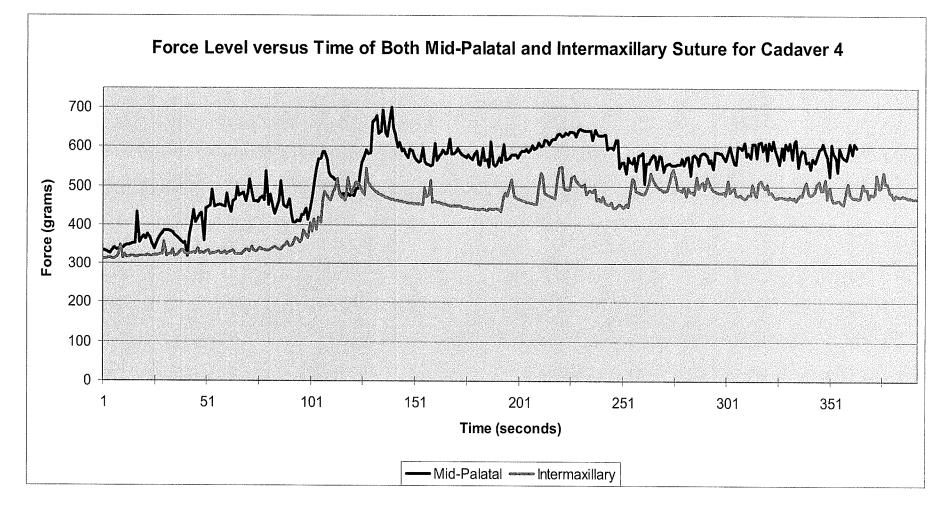


Figure 15: Force level (grams) versus time (seconds) of both mid-palatal and intermaxillary suture for cadaver 4

5.5 Mid-Palatal Suture Comparisons

A comparison of the mid-palatal sensor site results of all cadavers tested (1 through 4) is displayed by Figure 16. It is apparent that Cadaver 4 produced the lowest force values while Cadaver 2, the highest. This is also described in Table 5. Another interesting observation is that Cadavers 2, 3 and 4 appear to follow the same logarithmic trend in increasing force levels in the 2 phase of RME activation. Although Cadaver 1 also shows an increase, it is more gradual as compared to the others. Finally it is apparent that Cadaver 1 was the longest test to perform, while Cadaver 4 was the shortest. Using the unpaired t-test, we find that there is no statistical significance between cadavers for the maximum and minimum force values obtained.

	Maximum	Minimum	Difference
Cadaver 1	980.27	319.18	661.09
Cadaver 2	1152.42	461.36	691.06
Cadaver 3	1112.05	361.46	750.59
Cadaver 4	701.59	319.44	382.15

Table 5: Maximum and minimum force values (grams) of the mid-palatal sensorsite for all cadavers

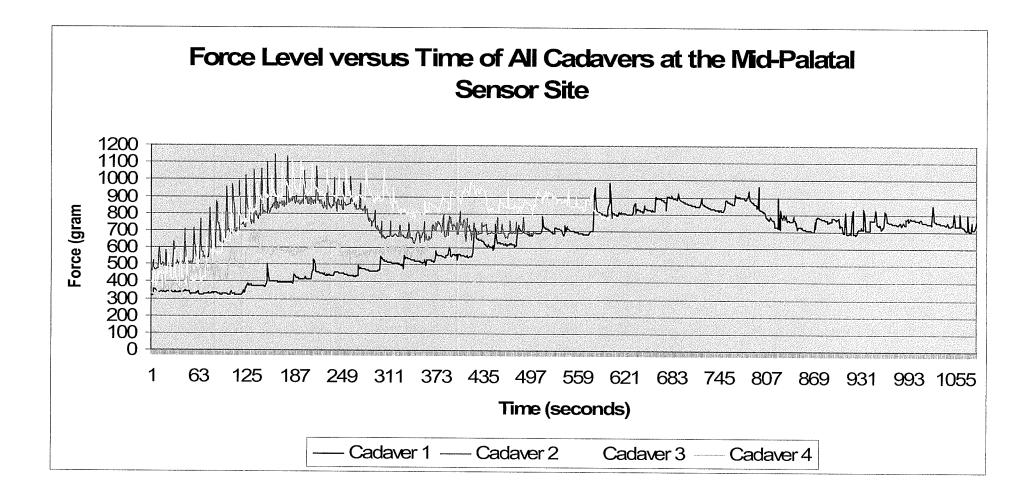


Figure 16: Force level (grams) versus time (seconds) of mid-palatal suture for Cadavers 1-4

5.6 Intermaxillary Suture Comparisons

A comparison of the intermaxillary sensor site results of all cadavers tested (1 through 4) is displayed by Figure 17. It is apparent that Cadaver 4 produced the lowest force values while Cadaver 1, the highest. This is also described in Table 6. Although all cadavers appear distinct, it appears that aside from Cadaver 3, the rest appear to follow the same logarithmic trend in increasing force levels in the 2 phase of RME activation. Finally it is apparent that Cadaver 1 was the longest test to perform, while Cadaver 4 was the shortest.

Using the unpaired t-test, we find that there is no statistical significance between cadavers for the maximum and minimum force values obtained (P<0.05).

	Maximum	Minimum	Difference
Cadaver 1	862.89	111.58	751.31
Cadaver 2	835.84	357.22	478.62
Cadaver 3	792.49	199.55	592.94
Cadaver 4	548.77	312.63	236.14

Table 6: Maximum and minimum force values (grams) of the intermaxillary sensorsite for all cadavers

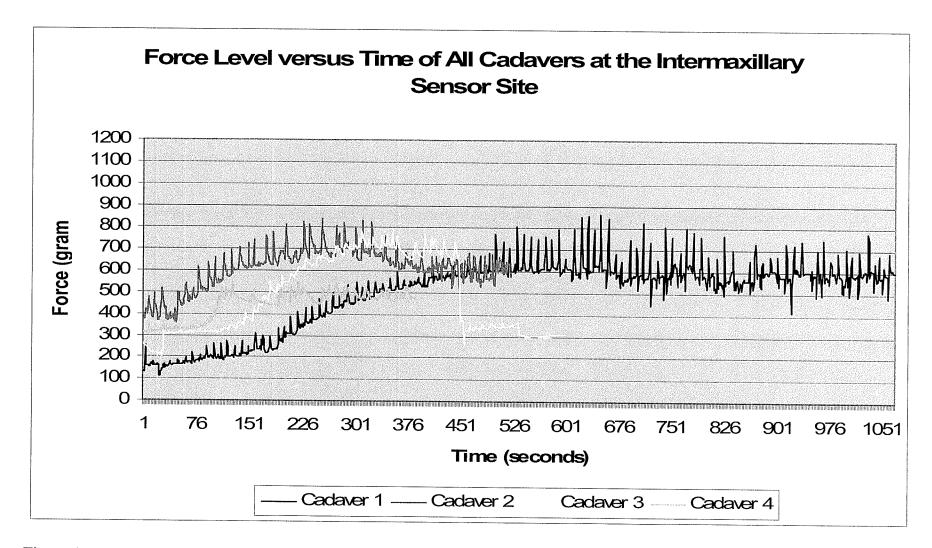


Figure 17: Force level (grams) versus time (seconds) of intermaxillary suture for Cadavers 1-4

5.7 Statistical Analysis of Maximum Force Values of both the Mid-Palatal and Intermaxillary Suture Sensors Sites

Maximum force values of all cadavers were compared for statistical significant differences using a two-tailed, paired Student t-test. A paired t-test is used when each data point in one group corresponds to a matching data point in the other group. The paired t-test is used to investigate the relationship between two groups where there is a meaningful one-to-one correspondence between the data points in one group and those in the other, e.g. a variable measured at the same time points under experimental and control conditions. Two-tailed tests are used where there is no basis to assume that there may be a significant difference between the groups (Hassard, 1991). It was determined that there was a statistical significance of the maximum force values between the mid-palatal and intermaxillary sensor site at the 95% confidence interval (p<0.05).

6.0 **DISCUSSION**

6.1 Main Discussion

Despite the extensive research of the effects of the RME appliance, this is the first study that measured the strain and force exerted directly on the bone in the human cadaver while activating an RME appliance.

Force values obtained for both the mid-palatal and intermaxillary sites exhibit values that were well within the range of orthopaedic values (over 500 grams). There were however differences between cadavers, as well as statistically significant differences due to different sites of measurement. The differences are understandable however, as there is individual variation from specimen to specimen. Each cadaver is unique, but follows a general trend of increasing force levels once the RME is activated. It can be postulated that these differences result from the individual variation between cadavers. Different cadavers have varying degrees of thickness of bone and soft tissues. Gender may also play a role in the different numbers, as the female cadavers were generally smaller than the male cadavers. Gender was not used in our analysis and as there was no objective way available to us to determine the hard and soft tissue thickness of each cadaver, accordingly we did not include that in our study. Some values did produce some anomalies in the graphing of the force versus time, specifically in Cadaver 3 and Cadaver 4. In Cadaver 3, at approximately 450 seconds, the RME appliance slipped off the Cadaver's oral cavity producing the jump as displayed in Figure 14. It was determined that the experiment did not have to be redone, as it took place in the end phase of the expansion. In Cadaver 4, there were some teeth that fractured as the expansion was

taking place, and as a result, the graph does not follow a gradual increase over time, especially in the first part of the expansion (phase 1 and 2). It is not expected that in a living subject the same type of teeth fracture will occur, due to the elastic fibers in the living subjects, vitality of the PDL and blood supply.

The mid-palatal sensor reading displayed some interesting rises and drops near the beginning of activation of the RME appliance. This may be attributed to one of the teeth fracturing during activation at approximately that time.

All sutures were given a visual and tactile examination following complete activation which yielded in no sutures having disconnected from one another or fractured despite the 12 mm of activation of the RME appliance. The use of UV light could have provided a bit more insight into the status of the sutures, as was performed by Gardner in 1971, but we opted for only gross evaluation with the naked eye. Furthermore, histological sections could have confirmed the extent of obliteration of the mid-palatal suture as was performed by Melsen in 1975. It would have been interesting to compare our results to her study, however due to the Department of Anatomy's policy governing these cadavers, we were unable to carry this out, as the cadavers were required by other health-care disciplines for routine dissection. Future studies on recently deceased cadavers, prior to rigor mortis or embalming could give some more insight into the histological aspects, as live studies on humans would not be possible. Although these studies would be ideal, it is not expected that they would be necessary as the studies of Ten Cate and Freeman (1977) have extensively examined this subject in rats. That being said, it would be

interesting to evaluate whether or not these specimens have sutures that are fused or if there is an ability to induce patency post-mortem with an RME.

When comparing the 2 sites of sensor placement specifically, it was noted the force levels at the mid-palatal sensor site produced statistically significant higher values than the intermaxillary sensor site. An analogy for this phenomenon is similar tat occurs during an earthquake. Although the epicentre has the highest value on the Richter scale, as you move away from the epicentre, the force of the earthquake weakens. This is exactly what happened in this study. Although not yet published, our study involved placement of more sensors at varying site throughout the craniofacial complex. It was found that those sensors that were placed further away from the RME device, the less amount it registered on the P3 measuring device. This confirms Isaacson's study from 1964, which gave similar findings. This gives more validity to the theory that orthopaedic forces can have an indirect effect on changes in the craniofacial skeleton through biochemical and/or cellular effects.

According to Buckland-Wright in 1978, sutures can absorb a considerable amount of energy, which is what we also found in our study. If this were not the case, the force levels would continue to increase higher and higher with no relaxation or fall in the values as time went on. Indeed there were general trends of increases over time, but they levelled off in all of our trials suggesting that not only the sutures, but the surrounding soft tissues play a role in force dissipation across the craniofacial osseous and non-osseus regions.

Despite the large forces exerted at these suture sites, no sutures were displaced or achieved patency in our study. Although a study by Wehrbein and Yildizhan (2001) analyzed the sutures of 18-38 year-old cadavers and found fusion had not actually occurred, our cadavers were much older. Also according to Wehrbein and Yildizhan, different patients exhibited different degrees of suture obliteration, so this variability should be accounted for when the clinician decides on using an RME for clinical practice. This was also found by Persson and Thilander in 1977 who actually found a 54 year-old subject without ossification. Furthermore, even if the mid-palatal suture did break, in elderly specimens, there is also resistance at the pterygomaxillary interface from the pterygoid plates of the sphenoid bones, which have a tendency to bend laterally and prevent the posterior area of the suture from opening (Wertz, 1970; Chaconas and Caputo, 1982; Jafari, Shetty and Kumar 2003). This resistance can further block any sutures from effectively opening and achieving orthopaedic expansion. This is why during SARPE procedures, the severance of the pterygomaxillary connection is necessary to properly achieve expansion. As the mode of action with RME appliances, the opening of the suture generally follows a fan-shape with larger opening in the anterior area and less in the posterior. This may indicate a higher force value in the anterior area or less resistance to expansion. This did not seem to be the case with our study, as the anterior area generated less force than posteriorly. Also, anatomy probably plays a role in this fan-shape expansion as there is only soft tissue anteriorly and posteriorly there are more hard tissue structures that can impede or lessen the effect of expansion, despite the force

acting directly in the area. This probably accounts for the higher force generation in the palatal area.

From the study of Isaacson and coworkers in 1964, strain gauges in RME's found that large forces of 1.3-4.5 kg were achieved from single activations with rapid decay initially. Zimring and Isaacson (1965) found that these forces were even higher in another study (7.5-15.7 kg). Although our numbers did not produce values as high as these, it could be because Isaacson and coworkers put the sensor directly on the RME, whereas our sensor was directly on the bone. This difference can therefore be postulated that the force was dissipated by all surrounding structures, including hard and soft tissues.

In the photoelastic study of Chocanos and Caputo study of 1982, it was found that the stresses generated in the anterior region of the palate were higher and became less and less as one moved more posteriorly. This was not the case in our study as the forces generated in the anterior area were significantly less than the posterior area (P<0.05). The explanation for this could be that Chaconas's study involved a plastic simulation of a human skull and did not factor in the effect of soft tissue which our study controlled for. However, that being said, Chaconas et al found that the forces generated were orthopaedic in nature which was also found in our study. Regardless, it is considered appropriate to generate higher forces in older patients requiring RME so that the force can be used to achieve some orthopaedic change, as Isaacson described in 1964.

From the work of Oberheim and Mao in 2002, it was found that bone strain was higher in younger skulls than in older skulls. Using this study as an example, it would be fair to assume that the forces generated from our study would result in even higher force values in younger patients due to their bone being less stiff than adult bone and subject to greater deformation. However, according to the finite element analysis study of Holberg et al in 2006, they displayed higher cranial base stresses due to the decrease in elasticity of the adult skull versus the young skull.

Our study also agreed with the findings of Timms' (1980) research. We also found the stress to be greatest in the area it is being delivered, while further away, it diminishes.

6.2 Study Assumptions and Limitations

Many assumptions were made while conducting this study. First and foremost, craniofacial orthopaedics is commonly attempted in the adolescent population and therefore a study on adolescent cadavers and dry skulls would be desirable. However they were not available for this study. Nevertheless, with the current upsurge in adult orthodontics, this study, despite the age of the cadavers, may have direct and important clinical applicability for dissipation of higher forces in general.

Secondly, we are making the assumption that the bone physiology of a cadaver that is fixed with formaldehyde will react similarly to that of a living subject. This is as close to the real situation as we are able to achieve.

Lastly, the sample size in this study could be considered relatively low. Performing this study involves many technique sensitive steps with sensors that were expensive and non-user-friendly which failed often. This combined with the fact that it requires 2 operators approximately 15 hours per cadaver to complete one study, makes it very time consuming. There was also a limit to the cadaveric material available at a short window of opportunity to conduct the experiment prior to dissection of the material by students.

The limitations in working with human cadavers include access to the important areas to be studied in the craniofacial skeleton. Achieving clear access to the RME appliance once fully seated was extremely difficult and required patience and determination to activate and turn the key for expansion.

7.0 CONCLUSIONS

Objective #1: To quantify the force levels generated at the mid-palatal suture during activation of the RME appliance.

Null Hypothesis #1: There are no measurable force levels detectable at the mid-

palatal suture after activation of the RME.

<u>There is sufficient evidence to reject null hypotheses #1 because it was found that</u> there were force levels detectable at the mid-palatal suture.

Null Hypothesis #2: The force levels generated at the mid-palatal suture are not orthopaedic in nature (500 grams/16 oz or higher).

<u>There is sufficient evidence to reject null hypotheses #2 because it was found that</u> there the force levels were orthopaedic in nature, or over 500 grams.

Null Hypothesis #3: The maximum force levels generated at the mid-palatal suture

do not exhibit statistically significant differences between cadavers.

<u>There is sufficient evidence to accept null hypotheses #3 because it was found that</u> <u>the maximum force levels did not differ with statistical significance at the mid-</u> <u>palatal suture between cadavers.</u>

Objective #2: To quantify the force levels generated at the intermaxillary suture during activation of the RME appliance.

Null Hypothesis #4: There are no measurable force levels detectable at the intermaxillary suture after activation of the RME.

<u>There is sufficient evidence to reject null hypotheses #4 because it was found that</u> there were force levels detectable at the intermaxillary suture.

Null Hypothesis #5: The force levels generated at the intermaxillary suture are not

orthopaedic in nature (500 grams/16 oz or higher).

<u>There is sufficient evidence to reject null hypotheses #5 because it was found that</u> there the force levels were orthopaedic in nature, or over 500 grams.

Null Hypothesis #6: The maximum force levels generated at the intermaxillary suture do not exhibit statistically significant differences between cadavers.

<u>There is sufficient evidence to accept null hypotheses #6 because it was found</u> <u>that the maximum force levels did not differ with statistical significance at</u> <u>the intermaxillary suture between cadavers.</u>

Objective #3: To determine if the mid-palatal suture remains fused or separates following activation of the RME appliance.

Null Hypothesis #7: The mid-palatal suture will not break following activation of the

RME appliance due to the advanced age of the specimens.

<u>There is sufficient evidence to accept null hypotheses #7 because it was found that</u> the mid-palatal suture did not break following activation of the RME appliance.

8.0 **REFERENCES**

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9.0 **APPENDICES**

9.1 Microsoft Excel Principal Strain Calculation Template

 Pricipal Strain Calculation

 Left Tube

 F_A
 45

 0
 0

Modulus of		
Elast.	29000	ksi
Poison's Ratio	0.29	

	E ₁	0.0000E+00
Strain LH	E ₂	0.0000E+00
	E ₃	1.0000E-06

		Actual	Micro
Princ. Strain	Р	1.2E-06	1
Ep,q (ε)	Q	-2.1E-07	0

Plain Stress (σ)	Р	0.0	ksi
	Q	0.0	ksi
Shear Stress (T)	Max.	0.0	ksi
Shear Stress (1)	Mean	4.7	ksi

	Calculated	22.5
Angle O (deg)	P	-67.5
	Q	22.5

9.2 Complete Raw Data for Cadaver 1

9.2.1 Mid-Palatal Suture Sensor

lime		2	3	100	43
1	-3	-3	-2	101	43
2	2	1	-3	102	47
3		3	-6	103	48
1	15	92	-565	104	47
5	13	71	-481	105	46
5	12	73	-484	106	43
7	<u> </u>	74	-482	107	43
<u> </u>	9	44	-294	108	41
)	9	42	-293	109	42
0	9	41	-293	110	-40
1	9	41	-290	111	40
2	8	41	-291	112	40
3	8	41	-292	113	40
4	2	38	-290	114	39
5	6	34	-246	115	39
6	5	31	-243	116	38
7	1	32	-243	117	37
8	6	34	-244	118	39
9	7	32	-243	119	
20	5	32	-242	120	49
1	3	31	-241	121	79
2	3		-241	122	57
3	3	32	-241	123	62
4	3	32	-241	124	60
5	3	33	-241	125	55
6	2	33	-241	126	67
7	2	33	-241	120	83
8	3	33	-240	128	78
<u>8</u> 9	3	33	-240	129	79
0	8	33	-241	130	79
1	13	36	-262	130	75
2	7	36	-262	131	77
3	16	30	-295	132	76
4	8	42	-295		
5	7	39	-246	134	75
6	5	39		135	
7	2	36	-245	136	74
	5	22	-244 -224	137	73
8				138	73
9	3	38	-255	139	72
0	3	37	-257	140	72
1	-9	34	-261	141	71
2	9	43	-269	142	71
3	2	37	-259	143	71
4	5	35	-276	144	
5	-5	40	-275	145	70
6	6	40	-310	146	68
7		45	-302	147	70
8	3	47	-304	148	68
9	-1	44	-295	149	66
)	1	49	-303	150	65
	2	50	-297	151	82
2	19	53	-294	152	93
1	10	50	-285	153	106
1	10	49	-284	154	109
5	10	49	-284	155	100
i .	. 10	49	-283	156	95
1	10	49	-284	157	99
3	9	50	-284	158	101
)	9	50	-284	159	100
	7	44	-269	160	99
·	7	43	-280	161	99
	0	42	-284		97
2	22	42		162	
, ,	33	42 49	-299	163	96
	30		-312	164	95
; ;		66	-373	165	94
	30	60	-359	166	93
		58	-357	167	93
	28	58	-353	168	92
)	28	58	-353	169	91
)	27	58	-353	170	91
	27	58	-353	171	90
	26	58	-353	172	89
-	26	58	-353	173	89
	26	58	-353	174	89
	20	55	-350	175	88
		57	-352	176	88
	23	56	-350	177	87
	24	57	-351	178	\$7
	24	57	-350	179	87
	20	52	-354	180	86
	21	53	-351	181	86
	22	52	-334	182	85
	18	46	-322	183	85
	17	41	-304	184	84
	21	49	-350	185	84
	21	43	-312	185	84
	20	38	-287	187	142
	20	38	-287	187	
					135
		37	-277	189	132
	20		-300	190	122
	20	44	200		120
7]]	20 24 43	44 46	-288	191	
7 3 9 1	20 24 43 43	44 46 52	-288 -303	192	119
	20 24 43 43 40	44 46 52 52	-288 -303 -321	192 193	119 118
	20 24 43 43 40 41	44 46 52 52 52 44	-288 -303 -321 -242	<u>192</u> <u>193</u> <u>194</u>	119
	20 24 43 43 40 40 41 43	44 46 52 52 44 54	-288 -303 -321 -242 -300	192 193	119 118
	20 24 43 43 40 40 41 43 45	44 46 52 52 44 54 56	-288 -303 -321 -242 -300 -298	<u>192</u> <u>193</u> <u>194</u> <u>195</u> <u>196</u>	119 118 116
	20 24 43 43 40 40 41 43 45 45 45	44 46 52 52 44 54 56 56 56	-288 -303 -321 -242 -300 -298 -298	<u>192</u> <u>193</u> <u>194</u> <u>195</u> <u>196</u>	119 118 116 115 114
5 7 7 9 9 9 9 9 9 9 9 9 9 8 5 5 7 7	20 24 43 43 40 40 41 43 45	44 46 52 52 44 54 56	-288 -303 -321 -242 -300	<u>192</u> <u>193</u> <u>194</u> <u>195</u>	119 118 116 115

100	43	48	-28
101	43	43	-70
102 103	47	50	-33
104	40	42	-28
105	46	36	-1.5
106	43	34	-22
107	43	36	-22
108	41	35	-23
109	42	32	-22
110	40	30	-23
111	40	31	-22
112	40	30	-22
113	40	29	-22
114	39	27	-21
115	39	27	-21
116 117	38 37	27	-21
118	39	28 32	-21
119	37	33	-23
120	49	33	-25
120	79	39	-27
122	57	35	-26
123	62	47	-30
124	60	49	-13
125	55	48	-13
126	67	46	-13
127	83	38	-11
128	78	50	-16
129	79	53	-16
130 131	79	54	-16
131	78	54	-16
132 133	77	54	-16
133 134	75	55	-16
135	74	55	-16 -16
136	74	55	-16
137	73	56	-16
138	73	56	-16
139	72	56	-16
140	72	56	-16
141	71		-16
142	71		-16
143	71	57	-16
144	70	57	-16:
145	70	56	-16
146	68	62	-18
147	70	64	-18
148	68	64	-18
149 150	66	59 57	-16
150	82	46	-166 -14:
152	93	52	-12
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54	109	27	-13
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56 57 58	99 101	59	-15
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203	101	42	-4.
205	100	44	-81
206	99	45	-82
207	98	43	-70
208	99	44	-74
209	97	43	-71
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211	124	33	-35
212 213	109	16	<u>15</u> 24
214	153	20	11
214 215	146	23	-24
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217	154	54	-14
218	152	56	-14
219	151	57	-14
220	150	. 57	-14
221 222	149	58	-15
223	147	58	-15
224	145	59	-15
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229	140	55	-17-
230	138	60	-16
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235	136	53	-14
237	133	52	-14.
238	133	52	-13
239	133	54	-149
240	162	44	-169
241	172	72	-253
242	174	83	-276
243	172	80	-27(
244 245	170	79	-26
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247	166	79	-265
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249	164	80	-264
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254	158	79	-26.
255	158	79	-262
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258	157	77	-275 -277
259	155	76	-275
260	147	64	-219
261	145	59	-206
262	144	60	-208
263	143	59	-208
264	142	59	-207
265	141	59	-206
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267	140	56	-195
268	139	55	-193
269	141	57 59	-199
270 271	143 146	<u> </u>	-195
272	200	59	-221
273	201	64	-199
274	202	72	-266
275	200	74	-272
276	198	74	-272
277	197		-273
278	195	75	-274
279		75	-274
280	193	76	-275
281	192	76	-275
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283	189	77 77	-276
285	189	77	-276
286	182	75	-276
287	179	73	+275
288	183	75	-276
289	183	74	-276
290	181		-280
291	181	75	-275
292	177	66	-244
293	173	67	-222
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321 213 77	-213
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324 211 77	-213
325 210 77	-212 -212
326 209 77	-212
327 209 78	-212
328 204 76	-215
329 204 76	-199
330 208 88	-326
331 199 79	-284
<u>332 252 51</u> <u>333 255 68</u>	-191
<u>333</u> <u>255</u> <u>68</u> <u>334</u> <u>257</u> <u>79</u>	-266
<u>334</u> 257 79	-273
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337 256 84	-287
338 254 85	-288
339 253 85	-289
340 251 86	-288
<u>341 250 86</u>	-289
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<u>352</u> 238 88	-288
<u>352 238 85</u> 353 238 90	-303
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357 226 66	-225
358 223 61	-219
359 225 54	-170
360 236 104	-409
361 229 68	-194
362 229 67	-190
363 229 67	-191
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366 226 67	-190
367 226 67	-190
368 225 67	-190
<u>369 224 66</u>	-190
370 224 66	-190
371 223 62	-215
372 222 57	-182
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9.2.2 Intermaxillary Suture Sensor

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9	-6 -7	19	14
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11	-5	22	15
12	-5 -1	31 26 21	-7 -8 -7 -7 -7 -7 -7 -7 -7 -7 -7 -7 -7 -7 -7
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14	-4 -5 2 -3 -4 -4 -4 -4 -4 -3	21	15
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354 355	2	343 343	198
356	4	345	197
357 358	4 8	344 350	196
359	8	360	205
360 361	4	357 424	205
362	-5	357	205
363	-2	355	202
364365	-3 -2	353 352	202
366	-2	351	202
367 368	-3 -4	351 350 350	203
369	-2	356	202
370 371	-16	370 397	207
372	-7	369	212 203
373 374	-5	368	204
375	-11	360	186
376	-7	364 365	193 198
378	-3	371	202
379 380	-40	370 386	199
381	-9	386	214 206
382	-11	373	201
383 384	-10 -10	373 373	201 202
385	-9	378	204
386 387	-7 -8	391 383	207 206
388	.9	378	204
389 390	-7 -11	383 384	207
391	-18	413	207 218 220 208
<u>392</u> 393	-18 -17	385 384	208
394	-17	384	207
395 396	-15 -27	382 374	197 200
397	-25	377	194
398 399	-25 -25	384	191
400	-39	435 383	227 191
401 402	-36	381	192
403	-31	384 383	<u>193</u> 192
404	-29	391	197
405 406	-22 -22	414 409	202
407	-15	420	205
408 409	-13 -20	417 419	210 207
410	-18		206
411 412	-15 -43	431	214
413	-27	447	219
414	-26	416	204
416	-21 -20	420	214
417	-19	420	214
418 419	-26	412 413	202 202
420	-24	413	205
421 422	-15 -58	438	210
423	-58	421 417	235 204
424 425	-18	432	205
	-18	432 431	205
426	-18		
426 427	-18	427	199
426 427 428	-22 -22	427 426	199 198
426 427	-22	427	199

432	-64	446	234
433 434	-32 -31	437 436	202
435	-32	433 440	199
436 437	-28	428	214
438 439	-35	427 439	195 211
440	-30	448	201
441 442	-29 -44	472 459	239
443 444	-37 -38	445	201
445	-38	442	199
446 447	- <u>37</u> -38	442	199
448	-39	440	196
449 450	-51	427 444	196 212
451	-63	438	206
452 453	-35	446438	195
454 455	-86 -74	447	246
456	-43	416 434	220 196
457 458	-43 -42	435 437	196
459	-43	436	198
460 461	-42 -26	442	199 224
462	-60	442	243
<u>463</u> 464	-38 -40	471 456	202
465	-38	456	196
466 467	-37 -36	458 458	201 200
468 469	-32	479 461	205
470	-32	486	209
471 472	-134 -70	460 469	269 216
473	-50	466	204
474 475	-49 -50	465 463	205 205
476 477	-49 -49	463 462	203
478	-44	480	204
479 480	-36 -95	533 457	232 232
481	-57	465	205
482 483	-55 -57	465	204 204
484	-55	464	208
485 486	-55	463	205 207
487 488_	-56 -53	463	206 213
489	-81	476	214
490 491	-56	461 503	203
492	•62	535	266
493 494	-90	470 468	226
495 496	-63 -66	470 468	208 209
497	-64	468	208
498 499	-66 -63	468 476	212
500	-68	476	215
501 502	-75 -47	634 545	296 259
503 504	-72 -74	484 480	213
<u>505</u>	-72	480	216
506 507	-73	478	215 212
508 509	-76	475	214
510	-73 -76	486	217 214
<u>511</u> 512	-66 -74	522 587	225
513	-107	453	231
514 515	-87	475 473	215 212
516	-85	474	212
<u>517</u> 518	-84 -88	475 442	211 219
519	-112	452	215
<u>520</u> 521	-70	580 550	253
522 523	-104 -92	449 474	214 211
524	-92	475	213
525 526	-93 -95	473 472	213 215
527	-97	481	221
528 529	-90 -109	504 467	239 219
530 531	-96 -85	486	225
532	-126	657 523	327 293
<u>533</u> 534	-101 -103	484 482	220 221
535	-101	483	219
536 537	-104 -103	480	222 219
538 539	-101	489	229
540	-104 -100	487 504	226
541 542	-78 -154	639 521	294 271
543	-125	486	220

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546	-114	483	22(
547 548	-113	483 483	220
<u>549</u>	-115	495	231
<u>550</u> 551	-108 -103	512 622	233
<u>552</u> 553	-171	494 480	272
554	-122	476	222
<u>555</u> 556	-122 -121	476	219 222
<u>557</u> 558	-122	477	219
<u>559</u>	-122	476 482	222 222
<u>560</u> 561	-108 -166	528 600	233
562	-111	470	227
<u>563</u> 564	-125 -126 -124	491	218 220
565	-124	493	221
566 567	-124 -124	492 493	220 223 221
568 569	-121 -123	495	221
570	-123	508	225
571 572	-104 -160	570	253
573	-121	<u>614</u> 518	339
574 575	-114 -115	490	216 218
576	-115	490	215
577 578	-116 -114	489 490	215
579	-114	490	215
580 581	-113 -92	499 623	227
582	-118	499	252
583 584	-113 -116	508	220
585	-116	504	216
586 587	-116 -120	<u>503</u> 499	214 213
588 589	-119 -123	500	215
590	-111	541	229
591 592	-111 -142	472	312 201
593	-138	478	211
594 595	-138 -137	479 480	213 209
596	-128	489	218
<u>597</u> 598	-125 -134	494 483	227
599	-143	490	218 220 257
600 601	-129 -111	529 516	257
602	-119	495	213
603 604	-118 -120	498 497	213
505 506	-118 -118	498	214
607	-118	499 498	215 213
<u>608</u> 609	-134 -143	487 425	226 224
510	-141	448	213
<u>511</u> 512	-137 -84	477 663	226 304
513	-143	569	280
614 615	-157 -142	486 474	218 219
516 517	-142	475	215
518	-143 -140	474 478	218
519 520	-151 -141	461 477	216
521	-152	433	224
522 523	-158 -85	443 693	231 311
524	-90	703	341
525 526	-172 -131	512 507	238 224
\$27	-132	503	223
528 529	-134 -133	<u>500</u> 501	223
\$30	-138	492	227
531 532	-176 -94	455 658	225 284
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534 535	-147 -121	480	218
536	-122	486	215
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539 540	-134	479	234
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542 543	-150 -104	498	248
544	-105	511 509	223
i45 i46	-104	509	218
47	-105 -107	507	218 220
i48 i49	-131 -124	484	228
	-69	563 726	270 326
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	-162 -109 -110 -109	499 491 490 493	212 212 212

656 657	-108	495	214
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660 661	-82	589	238 344
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666	-108	486 484	210
667	-109	483	210
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669 670	-105	466 485	216
671	-116	499	232
672	-124	529	297
673 674	-109	449	202
675	-103	465 466	202 204
676	-101	468	203
677	-102	467	203
678 679	-131 -120	400	207
680	-88	477 523	237
681	-178	413	241
682	-120	422	197 197
683 684	-112 -107	434	197
685	-107	440	197
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687	-110	440	197
688 689	-109	444 440	205
690	-110	456	202 203
691	-108	508	224
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693 694	-167	427	209 203
695	-103	454 458	201
696	-103	457	203
697	-101	460	202
698 699	-102	459 457	203
700	-104	457	202 207
701	-89	562	297
702	-48	516	243
703 704	-146 -97	396 461	200
705	-93	464	204
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707 708	-93	466	201
708	-94 -104	465	201
710	-118	446	203
711	-40	680	305
712	-130	433	197
713 714	-96	450	198 197
715	-97	449	198
716	-97	450	197
717 718	-98	453 447	201
719	-93	447	202
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722 723	-205	295 402	221 220
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727 728	-94	449	205
729	-100	439	204
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732 733	-100	<u>510</u> 424	262 205
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735	.92	459	203
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737 738	-91	461	205
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740	-137	338	193
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61	-95	451	228
62	-82	450	228
63	-78 -68	460 532	241
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64 65 66	-137 -83	409 446	249 216

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774 775	-62 -60	480	222
776	-53	493	230
777	-55	490	239
778 779	-55 -65	488	234
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781	-96	458	235
782	-40	633	307
783 784	-71 -87	472 439	244 211
785	-81	446	209
786	-79	447	209
787 788	-78 -80	448 446	215 214
789	-79	446	214 221
790	-110	399	225 232
791	-112	397	232
792 793	-67 -72	478	228
794	-39	586	322
795	-80	422	234
796 797	-79	442	216
798	-76	444 439	214 214
799	-81	439	213
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801	-131	380	226
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805	-131	377	249
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808	-73	444 452	215 224
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813	-124	390	203
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819	-94	418	195
820	-91	424	204
821 822	-89 -93	423 419	<u>198</u> 197
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824	-102	414	204
825 826	-136	357 614	202 297
827	-127	410	213
828	-88	432	197
829	-86	434	196
830 831	-87	435 437	<u>196</u> 198
832	-90	430	190
833	-95	439	200
<u>834</u> 835	-106 -83	448	190 206
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837	-79	469	222
838	-74	475	212
839 840	-102 -116	539 381	311 215
841	-104	385	213
842	-87	421	215
843 844	-98 -84	376 421	211
845	-90	417	216
846	-99	383	206
847	-93	365	208
848 849	-105 -80	<u>397</u> 414	211 212
850	-73	398	216
851	-95	376	206
<u>852</u> 853	-83	422	214
854	-93	426 433	211 208
855	-82	428	200
856	-81	429	196
857 858	-83 -82	428	199
858 859	-82	429 428	200
860	-81	428	200
861	-85	432	204
862 863	-81	515 365	251
864	-88	429	207
865	-84	432	198
866	-85	432	197
867 868	-97 -89	<u>386</u> 431	196 200
			200

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871	-41	587	253
872 873	-122 -68	446 457	226
874	-65	458	219
875 876	-68	455 453	219
877	-67	455	217
878 879	-110 -101	400 394	215
880	-68	482	203 252
881	-60	499	253
882 883	-72	447 448	212
884	-64	455	224
885 886	-63 -65	456	232 234
887	-62	457	229
888 889	-67 -70	451	222
890	-74	448	224
891	-72	474	231 244
892 893	-37 -76	526 483	244
894	-61	462	255 226 224
895 896	-58	465	224
897	-60 -58	463 464	224 225
898	-60	462	224 222
899 900	-59	462 452	222
901	-91	419	211
902 903	-122	510	308
903	-115 -73	376	236
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906 907	-73 -75	439	218
908	-72	440	212
909	-71	440	212
910 911	-72 -72	438	212
912	-108	364	215 212
91 <u>3</u> 914	-75 -31	<u>440</u> 572	235 283
915	-97	496	305
916	-79	413	217
917 918	-71 -69	433 436	215
919	-68	430	213 212
920	-68	438	215
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26	-45	583	270
)27)28	-61	465	228
029	-60	464 469	220
030	-56	470	232
)31)32	-64	459 460	222 214
933	-66	457	214
034 035	-72	456	216
036	-67 -33	455 588	211 259
37	-50	596	285
) <u>38</u>)39	-95	455 454	233 216
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141	-58	462	216
942 943	-56	463	215
44	-55	464	216
45 46	-56 -57	463	217
47	-55	463	214
48	-56	463	220
49 50	-73 -76	431 469	215
51	-88	380	204
<u>152</u>	-64	447	212
953 954	-64	449	212
55	-65	449	211
956 957	-68	453	217
157	-60	342 543	208 286
59	-79	554	263
960 961	-94 -57	404 461	240
62	57	461	212
63	-57	461	213
964 965	-56	462 351	212
66	-79	409	214
67	-95	445	277
68	-58	614	269

970	-64	437	215
971 972	-65 -65	435 439	218
973	-67	435	219
974	-75	428	212
975 976	-97	426 400	227
977	-124	466	314
978	-52	500	259
979	-52	482	248
980	-59	451	
981 982	-60	450 453	220
983	-59	451	218
984	-61	-449	218
985	-83	412	224
986	-82	427	215
987 988	-91 -67	456 539	251 276
989	-70	445	222
990	-68	443	219
991	-68	442	220
992	-67	442	216
993 994	-88 -109	425	228
995	-101	368 362	210
996	-71	397	214
997	-75	403	209
998	-89	397	213 247
999	-80	430	247
1000 1001	-76 -64	560 391	278
1002	-68	430	217 221
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1004	-102	346	205
1005	-94	410	239
1006	-83	427	229
1007 1008	-77 -73	<u>482</u> 537	243
1009	-87	449	255 225
1010	-74	436	226
1011	-72	435	225
1012	-73	433	223
1013 1014	-71 -72	436	224
1014	-72	435 434	227 230
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1018	-82	379	200
1019	-56	537	279
1020 1021	-61	457 445	229
1022	-60	443	219
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1024	-57	446	226
1025	-54	451	233
1026 1027	<u>-55</u> -61	449	233 237
1028	-55	454 449	237
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1031	-13	620	295
1032 1033	-24	597	286
1033	-81	429 455	245 243
1035	-54	457	243
1036	-55	455	240
1037	-54 -55 -55	455	241
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1039 1040	-94 -44	355 479	229
1040	-72	479	261 270
1042	-89	395	255
1043	-82	394	249
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1045	-79	407	256
1046 1047	-89	520	288
1048	-65	417	246
1049	-64	414	230
1050	-63	416	237
1051	-63	415	238
1052	-84	352	214
1053 1054	-70	442 457	263
1054	-61	45/	<u>265</u> 242
1056	-62	430	242
1057	-61	429	241
1058	-61	428	240
1059	-62	426	241
1060	-87	310	217
1061	-43	533	272
1062	-36 -53	486 452	248 245
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067	-51	448	238
068	-50	446	238
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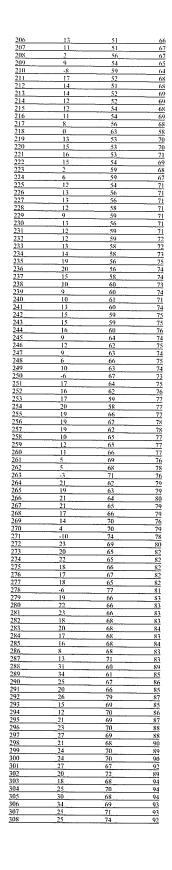
9.3 Complete Raw Data for Cadaver 2

9.3.1 Mid-Palatal Suture Sensor

time	1	2	3
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3	-6	0	8
4	-1	- <u>I</u>	
6	-4	0	$ \frac{4}{5} \frac{4}{6} \frac{6}{7} \frac{7}{8} \frac{10}{10} $
7 8		2	4
9	-3	0	7
10		<u></u>	8
12	0	-1	10
13	-3	4	11 8 8 10
14	-7 -17	5 6	<u>8</u> 10
$\begin{array}{c} 9 \\ \hline 10 \\ \hline 11 \\ \hline 12 \\ \hline 13 \\ \hline 14 \\ \hline 15 \\ \hline 16 \\ \hline 17 \\ \hline 18 \\ \hline 19 \\ \hline 20 \\ \hline 21 \\ \hline 22 \\ \hline 23 \\ \hline 24 \\ \hline 25 \\ \hline 26 \\ \hline 27 \\ \hline 28 \\ \hline 29 \\ \hline 27 \\ \hline 28 \\ \hline 29 \\ \hline 30 \\ \hline \end{array}$	-3	4	10
17	-2	4	10
19	0	4	<u>10</u> 10
20	1	6	11
21 22	-3	<u>6</u> 8	<u>11</u> 11
23	-4	<u>8</u> 7	<u>13</u> 13
24	-6	8	<u>13</u> 14
26	-4	× 7	14
27	-2	8	14 15
29	2	7 8	16 16
30	-9	12	12
31	-3	10	12 17 17
32 33 34	-5	10	16
34	-2	14	16 15 19
35 36 37 38	-1 3	5	19 21
37	1	10	18
38 39	2	12	18
<u>40</u>	2	10 12 13 11 13 11	<u>19</u> 21
41	1	13	21 21 22 23
$ \frac{42}{43} \\ \frac{44}{45} \\ \frac{46}{47} \\ \frac{47}{47} $	0	11	22
44	1	13 12 12 13 15 14	23
45	1	12	23
40	0	13	23
48	-3	14	23
48 49 50	-2	16	22
51	-9	15	23
52 53 54 55 56 57 58 59 60 61	-1	15	23 23 23 23 23 23 23 23 23 23 23 23 23 2
54	-1	16	24
55	0	18	25 24 24 27 27 27 27
56	0 3	17	24
58	1	15	27
59	1	17	27
61	-3	19 24	27 27 22 28 28 28 28
62 63 64 65 66 67 68 69 70 71	-1	19	28
<u>63</u>	0	18	28
65	1	20	28
66	0	19	27 28
<u>67</u> 68	-6 -2	20	29 30 30
69	-3	19 18 20 21 22 14	30
70	-3	22	29 32
72 73	-4	22	30
73	-1	21	32
74 75 76	-3	21	32
76	-3	23	32 32
77 78	-4 -2	23 21	32
79	-15	24	34
80 81	-9	27	32
82	-7	24	<u>32</u> 36
83	-1	23	35
<u>84</u> 85	-5 -15	26	<u>35</u> 34
86	-5	25	36
87 88	-5	25 25	36
89	-4	25	37
90	-5	25	37
91 92	-3	24	39
93	-5	26	39
94	1	26	40
95 96	-3	26	<u>39</u> 41
97	-2	28 26	40
98 99	-8	27 25	41
100	4	25	41 41
101	5	25	42
102	5	25	42

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104	8	26	42
105 106	<u> </u>	25	43
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109	7	27	44
<u>110</u> 111	9	30	45
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115 116	-7 3	33 30	43
117	3	31	43
118	4	30	44
119	4	30	42
120 121 122	<u> </u>	29	45
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123	8	29	45
124	0	32 32	44
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128	-4	28	-44
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133	-14	40	41
134	13	26	50
135	5	33	48
136 137	5	33	48 47
<u>137</u> <u>138</u>	0	33 34	47
139	-1	33	44
140	-4	39	44
141	-23	52	37
142 143		35	49
144	9	32	52
145	-2	41	36
146	- 6 - 7	36	50
147 148		36	50
148		<u>36</u> 49	<u>51</u> 37
150	8	36	52
151	8		52
<u>152</u> 153	8	37	52
<u>153</u> <u>154</u>	-1	<u>39</u> 40	<u>52</u> 52
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157	5	- 41	52
158 159	8	38	54
160	. 11	38	<u>54</u> 55
161	5	41	54
162	6	40	55
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164 165	<u>8</u> 6	40 44	<u>56</u> 51
166	8	41	56
167	11	40	57
168		40	57
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171	-1	43 45	<u>55</u> 57
172	5	42	58
173	5	45	55 57
174 175	4	45	57
175	03	48 44	<u>52</u> 46
177	8	41	59
178	4	49	58
179		45	59
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181		43	60
181 182	11		
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182 183 184	12	45 47	<u>60</u> 60
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182 183 184 185 186 187 188	12 7 9 11 11 7	45 47 46 45 45 47	60 60 61 61 60 60
182 183 184 185 186 187 188 189	12 7 9 11 11 7 9	45 47 46 45 45 45 47 47	60 60 61 61 61 61 61
182 183 184 185 186 187 188 189 190	12 7 9 11 11 7 9 9 9	45 47 46 45 45 47 47 47 47	60 60 61 61 60 61 60 61 62
182 183 184 185 186 187 188 189 190 191	12 7 9 11 11 7 9 9 9 9 12	45 47 46 45 45 47 47 47 47 47 46	$ \begin{array}{r} 60 \\ 60 \\ 61 \\ 61 \\ 60 \\ 61 \\ 62 \\ 62 \\ 62 \end{array} $
182 183 184 185 186 187 188 189 190 191 192 193	12 7 9 11 11 7 9 9 9 12 12	45 47 46 45 45 47 47 47 47 46 47	$ \begin{array}{r} 60\\ 60\\ 61\\ 61\\ 61\\ 60\\ 61\\ 62\\ 62\\ 62\\ 62\\ 62 \end{array} $
182 183 184 185 186 187 188 189 190 191 192 193 194	12 7 9 11 13 7 9 9 9 12 12 12 13 8	45 47 46 45 45 47 47 47 47 47 46 47 47 49	$ \begin{array}{r} 60\\ 60\\ 60\\ 61\\ 61\\ 61\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62 \end{array} $
182 183 184 185 186 187 188 189 190 191 192 193 194 195	12 7 9 11 11 7 9 9 9 12 12 13 8 8	45 47 46 45 47 47 47 47 47 47 47 46 47 47 47 49 48	$ \begin{array}{r} 60\\ 60\\ 61\\ 61\\ 61\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62$
182 183 184 185 186 187 188 189 190 191 192 193 194 195 196	12 7 9 11 11 7 9 9 9 12 12 13 8 8 8 10	45 47 46 45 45 47 47 47 47 46 47 47 46 47 47 49 49 48 49	$ \begin{array}{r} 60\\ 60\\ 60\\ 61\\ 61\\ 60\\ 61\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63$
182 183 184 185 186 187 188 189 190 191 192 193 194 196 197	12 7 9 11 11 7 9 9 9 9 12 12 12 13 8 8 8 10 12	45 47 46 45 45 47 47 47 46 47 47 47 47 47 49 48 49 48	$ \begin{array}{r} 60\\ 60\\ 61\\ 61\\ 61\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 63\\ 64\\ 64\\ \end{array} $
182 183 184 185 186 187 188 190 191 192 193 194 195 196 197 198	12 7 9 11 11 7 9 9 12 13 8 8 8 8 10 12 12	45 47 46 45 45 47 47 47 47 47 47 47 47 47 47 49 48 49 48 49 48 49	$ \begin{array}{r} 60\\ 60\\ 61\\ 61\\ 61\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63\\ 63$
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182 183 183 184 185 186 187 188 190 191 192 193 194 195 196 197 198 199 200 201	12 7 9 11 7 9 12 13 8 10 12 13 8 10 12 13 12 13 12 13 12 13 12 13 12 13 14	45 47 46 45 45 47 47 47 47 47 47 47 47 47 47 47 49 48 48 49 49 47 48 48 49 47 48 8 49 47 48	$\begin{array}{r} 60\\ 60\\ 60\\ 60\\ 61\\ 61\\ 61\\ 61\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62$
182 183 184 185 186 187 188 189 190 191 192 193 194 195 196 197 198 199 200 201 202	12 7 9 11 7 9 12 13 8 10 12 13 8 10 12 13 12 13 12 13 12 13 12 13 12 13 14	45 47 46 45 45 47 47 47 47 46 47 47 46 47 49 49 49 49 48 48 48 48 48 48 48	$\begin{array}{r} 60\\ 60\\ 60\\ 61\\ 61\\ 61\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 63\\ 63\\ 64\\ 61\\ 65\\ 65\\ 65\\ 65\\ 65\\ 65\\ \end{array}$
182 183 183 184 185 186 187 188 190 191 192 193 194 195 196 197 198 199 200 201	12 7 9 11 11 7 9 9 9 12 12 13 8 8 8 10 12 12 12 12 13 12	45 47 46 45 45 47 47 47 47 47 47 47 47 47 47 47 49 48 48 49 49 47 48 48 49 47 48 8 49 47 48	$\begin{array}{r} 60\\ 60\\ 60\\ 60\\ 61\\ 61\\ 61\\ 61\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62\\ 62$

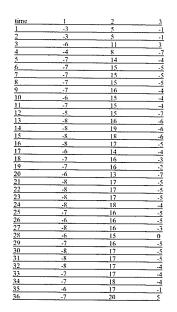


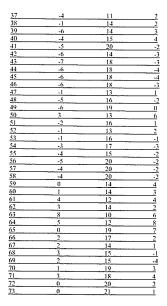
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317 318	29	74	95
319	30	75	95
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321	22	77	95
322 323	26	77	<u>96</u> 97
323	31	74	97
325	30	78	96
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	28	77	97
328 329	<u>31</u> 13	75	97
330	13	<u>89</u> 77	93
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332	38	72	99
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334	. 41	72	101
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337	30	70	99
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342	22	77	104
343	28	77	101
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345	35	74	103
346 347	25 36	81 74	<u>96</u> 103
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351	40	73	104
352 353	35 30	76	<u>104</u> 105
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381	36	82	109
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387	19	89	108
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417	38	89	116
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420	41	89	116
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423 424	46	88	118
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425 426	35	93	116
426	43	90 90	117
427		90	118
428 429	40 39		118
429		91	119
430		91	117
431 432	43	89	122
	44	88	120 121
433	48	89	121
434	45	88	122
435	47	88	122
436	49	87	122
437	40	89	122 122 122 122 122 121
438	42	89	121
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440	47	87	123

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443	38	97	11
444	43	90	12
445	46	92	12
446	45	88	11
447	27	99	11
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449	41	91	12
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464	39		12
465	39	93	12
466	39	94	12
467	30	96	12
468	26	102	
469	35		11
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471	40	94	12
472	40	94	12:
472	38	95	12 12
474	40	94	12
475	40	94	12
476	41	94	120
477	41	93	12.
478	42	94	
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482	32	98	125
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494	42	95	123
495	42	95	124
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498	31	101	124
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500	28	96	. [19
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502	40	97	124
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503 504	44	90	126

9.3.2 Intermaxillary Suture Sensor





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77	0	21	6
78	-1	20	8
79	0 -1 -2 -2	19	5
80	-2	21	7
81	1	21	
82	1	21	9
83	5	18	4
84	-1	24	7
85	-2	24	7
86	-2	24	7
87	-1	25	9
88	-1 -2 -2 -1 -2	20 21 20 19 21 21 21 21 21 21 24 24 24 25 24 25 24 24 25 24 24 26	10
89	-1 0	24	9
90	0	26	2
91	-4	26	7
92 93 94 95 96 97 98	-4 -3 -3 -3 -2 -1 0	26	7
93	-3	26	7
94	-3	26	7
95	-2	25	7
96	-1	25	9
97	0	26 26 25 25 25 23 26 26 26 24 26 26	10
98	-3 -2 0	23	7
99	-3	26	7
100 101	.2	26	8
101	0	24	8
102	-4	26	5
103	-4	26	8
104	-2	26	8
105	4 -2 0 -2	26 28	$ \begin{array}{r} 1 \\ 5 \\ 5 \\ $
106	-2	26	9
107	l	23	8
108	1	25	3
109 110	0	22	<u>8</u> 3 9
110	-6	28	-

111 112	-5	28 32	0
113	-4	30	5
114	-3	30	5
114 115 116	i 2	29	6
117		29	8
118 119	<u> </u>	23 28	7
120		30	8
121 122 123 124 125 126 127 128 129	-1	30	8
122	-!	<u>30</u> 30	8
124	-1	31	8
125	-1	32	7
126		32 32	4
128	-1	32 32	8
129 130	-1	32	
131	0	33	<u></u>
132	0	33	1
132 133 134	-2 -7	35	4-6
135 136 137	-14	44	-6
136	-6	39	3 4 5 4 4 4
138	-5	30	5
139	-5	39	4
140 141	-5 -4	38	4
42	-9	42	-6
43	-22	50	- 1
45	-12	44	
46	-10	44	-1
47 48	-8	41	<u>2</u>
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50	-20	51 53	-1 -9 -7
51 52	-17 -16	51 50	.7
52 53 54 55 56	-15 -16		-7
54 55	-16 -32	<u>51</u> 63	-1
56	-27	62	-2-
57 58 59 60	-23	58	- 1-
59	-22 -21	57	-1
60	-21 -20	57	-10
61 62	-20 -38	58 70	-1:
63	-28	64	
64	-27	63	-11
65 66	-27 -24	64 62	-11
67	-40	75	-1:
68	-33		-2:
69 70	-31	<u>69</u> 68	-23
71	-30	67	-22
72	-30 -32	<u>68</u> 71	-21
74	-40	77	-32
74 75 76	-39 -37	75	-29
77	-36	73	-27
78	-35	72	-27
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82	-40 -39	78	-31
83 84	-39	77	-30
85	-37	76	-26
86 87	-55	88	-42
88	-45	83	-37
89	-44	82	-34
20 21	-43	82	-32
2	-42	82	-37
03 04	-53 -48	94	-43
)5	-47	88	-40
)6	-47	86	-37
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)1)2	-55 -54	94 93	-46 -44
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)4)5	-50	91 104	-43
)6	-61	101	-50
)7	-59	97	-49
98 19	-55	99 97	<u>-45</u> -55
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4	-62	104	-50
5.	-61	103	-50
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8	-58	101	-48
9 0	-64 -65	109	-63
1	-65	108	<u>-60</u> -55
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226 227	-72 -76	115	-63
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229 230	-78	122 120	-66 -67
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232	-78 -83	127	-77
233 234	-82	126	-71
235	.79	124	-68
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241	-80	128 125 125 124 123	-72
241 242 243	-78	125	-67
<u>243</u> 244	-76	124	-65 -64
245	-75	123	-63
246 247	-75 -74	123	-62
248	-73	122	-58
249 250	-72 -71	121	-60
251	-70	120	-57
251 252 253	-68	119	-57
253	-67 -69	118	-54 -56
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265	-83	133 130	-63
266 267	-74 -71	124	-63
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273 274	-71 -68	124 121	-60
275	-68	121	-58 -59
276 277	-80	132	-67
278	-77	136	-70 -70
279	-78	131	-68
280 281	-77 -76	130	-66 -66
282	-73	127	-64
283 284	-73 -78	127	-64
285	-84	137	-73
286 287	-83 -82	137	-72
288	-81	137	-70
289 290	-77 -77	133	-68
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293 294	-92 -87	144	-75 -75
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302	-88	146	-76
303 304	-87 -85	145	-74
305	-84	142	-72
<u>306</u> 307	-84	142	-72 -73
308 309	-84	144	-75
309 310	-102 -95	158	-88
311	-91	155	-79
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	-94	155	-88
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317 318 319	-93	154	70
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317 318 319 320 321 322	-93 -93 -91 -90	154 155 152	-79 -75
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343 344	-81	154	-70
345	-81	152	-70
<u>346</u> 347	-77	150 150	-69
348	-78	150	-69
349 350	-76	149	-69
351	-74	149	-66
352 353	-76 -74	149 150 150	-67
354	-69	150	-66
355 356	-75 -74	150	-64
357	-74	150	-64
358 359	-73	150	-63 -63
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361 362	-68 -69	146	-63 -62
363 364	-67 -69	146	-62
365	-64	146	-64
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369 370	-68	147	-57
371	-67 -67	147	-57
372 373	-64	145	-57
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389	-59	144	-52
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410 411	-55 -51	143	-46 -46
412	-52	141	-47
413 414	-53 -54	143	-47 -45
415	-50	140	-45
416 417	-59	148	-58 -51
418	-59	149	-50
419 420	-59	149	- <u>50</u> -52
421	-60	150	-50
422 423	-53	143	-47 -48
424	-51	142	-47
425 426	-66	154	-62 -59
427	-65	154	-57
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452	-67	161	-53
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456 457	-67	161	-56
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463	-72	167	-58
464 465	-72	167	-57
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471	-71	165	-56
472 473	-67 -69	162	<u>-57</u> -57
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475	-68	163	-55
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478	-64	163	-50
479	-67	162	-52
480 481	-68	162	-52
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496 497	-66	163	-49 -48
498	-65	162	-46
499	-62	161	-45
500 501	-62 -64	161 162	-44 -46
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<u>503</u>	-65	167	-49
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507 508	-66 -62	165 163	-46
509	+62	163	-45
510	-60	161	-45
511 512	-61	161	-47
513	-61 -62	163	-44
514	-61	163	47
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567	-70	173	-55
568 569	-69 -68	172	-55
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<u>572</u> 573	-67 -66	172	-52
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<u>594</u> 595	-50	165	-45 -43
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605	-61	165	-45
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617	-49	159	-35 -36
618	-48	159	-36
619 620	-49 -54	161	-41
621	-51	160	-45
622	-50	159	-35
623 624	-46	157	-32
625	-46	156	-31
626	-45	155	-29
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630	-42	155	-34
631	-48	153	-21
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655	-2	115 115	13
656	-1	114	13 13 12
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658 659	-1 -2	115	<u>15</u> 13
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687 688	7	111	18 18
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701 702	12	110	22
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711	15	109	26
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735 736	20	109	31
130	19	108	<u>30</u> 31
738	20	109	31
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56 57	29	102	<u>39</u> 38
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64 65	28	102	<u>39</u> 39
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75 76	<u>31</u> 31	101	<u>39</u> 39
77	31	101	38
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79 80	27	101	<u>39</u> 39
81 82	28	103 98	38 40

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784	28	103	39
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820	38	100	55
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877	37	102	48
878	37	93	48
879	37	101	48

9.4 Complete Raw Data for Cadaver 3

9.4.1 Mid-Palatal Suture Sensor

1 13 -5 11 2 14 -4 13 4 15 -3 14 5 12 -4 21 6 21 -2 17 7 19 -3 17 9 19 -2 18 10 19 -2 18 11 20 -2 18 12 20 -2 19 13 21 -2 19 15 21 -1 19 16 22 -2 19 17 17 0 36 18 19 3 29 20 20 2 28 21 20 2 28 22 3 22 3 29 23 21 5 32 26 19 8 40 27 20 <	time	l	2	3
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<u>110</u> 111	52	17	72
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113 114	<u>52</u> 52	17	68
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121	56	19	72
122 123	<u>55</u> 55	19	<u>66</u> 47
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142	65 65	22	80
143 144	65	22 22	80
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147	67	21	81
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150	64	22	81
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152 153	57	18	85
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165 166	80	34 33	77
167	84	31	79
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169 170	-19	20 5	<u>84</u> 92
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180	50	19	83
181 182	63 80	29	<u>81</u> 80
183	84	34	80
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185 186	54	19 20	<u>85</u> 85
187	59	20	85 83
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196 197 198 199 200 201 202	61 62 63 54 54	17 17 18 14 16	72 73 73 73 73
196 197 198 199 200 201	61 62 63 54	17 17 18 14	72 73 73

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207 208	59	16	76 77 79 77 77 77 78 78 78
209	37	16	77
210 211	45	16	77
211 212	46	17	78
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215	58	18	78 79
216	58	18	79
217	56	19	79
218 219	<u>58</u> 57	19	79
220 221	58	19	79
221	57	18	81
222 223 224	52	2120	81
224	<u>54</u> 56	20	81
225 226	54 55	18	80
220	58	20	<u>80</u> 81
228	58	19	
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234	59 59	20	85
236	60	21 21	85
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262	60	22	86
263	60	21	89
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265 266	62	23	85
267	61	22	
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270	65	26 24	91
271	73	23	87
272 273	71	23 24	83
274	73	24	82
275	72	24	83
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278	73	25 25	83
279 280	74	26	83
280 281	74	26	. 83
281	74	26	83
283	74	26	84
284	75	26	
285 286	75	27	<u>84</u> 84
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288	75	27	
289 290	76	27	85
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291 292	76	27	86
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298 299	78 81	28	87
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301 302 303	78	28	88
<u>302</u> 303	78	29	88
304	79	29	89
305 306	79	29	89
306	80	27	88
307 308	72	<u>30</u> 30	<u>93</u> 93

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312	75	30	9.4
313 314	76	30	94
315	76	30	95
316 317	76	31	<u>95</u> 95
318 319	77	31	95
319 320	77	31	96
321 322 323 324	77	31	96
322	78	28	94
324	74	32 32	99
325 326	74	32	<u>100</u> 100
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332	74	31	103
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335	76	33	104
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342 343	77	33	<u>105</u> 106
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)78	233	-23	396
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)80)81	256	-4 -6	410
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182	292	-12	472
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189	294	0	487
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192 193	294	-8	478
	294	-10	465
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195 196 197 198 199	293 294 298	-28 -26 -8	449 512
195 196 197 198 199 200	293 294 298 300	-28 -26 	449 512 477
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264 265	315 313	25	581
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268 269	313 318	16	559 533
270	318	16	562
271	317	13	556
272 273	322 319	29 19	592
274	319	13	578
275	.319	15	563
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277 278	303	23	<u>592</u> 587
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1388	341	42	633
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1469	344	27 26	575
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1476	344	26	571
1477	344	25	571
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1484 1485	345	25	567
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1497 1498	<u>346</u> 345	22	<u>561</u> 560
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1501	344	15	553
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1506	346	19	552
1507	347	20	553
1508 1509	347	20	554
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1516	343	17	549
1517	346	18	549
1518	347	15	545
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1520	347	15	545

9.4.2 Intermaxillary Suture Sensor

time	11	2	3
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3	-15	1	61
4	-15	1	57
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6	-15	2	54
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8	-8	3	48
9	-18	1	49
10	-17	5	46
11	-9	4	40
12	-13 -15 -15 -15 -15 -15 -15 -11 -18 -17 -9 -2 -5	8	32
13	-5	12	35
14	1	9	29
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17	-12	4	36
18	-12	4	34
19	-10	4	34
20	-8	6	30
21	-15	7	24
22	-2	6	24
23	-14	6	29
24	-13	5	28
25	-12	5	27
26	-9	11	22
27	6	40	22
28	-3	-67	-30
29	2	-77	-19
10 11 12 13 14 15 16 17 18 19 20 21 22 23 24 25 26 27 28 29 30 31	-14 -12 -12 -12 -10 -8 -15 -2 -14 -15 -12 -12 -9 -6 -3 -3 -2 -2 -2 -2 -22	165	-48
31	42	170	-46
32	-4	162	-34
32 33	<u>-4</u> -3 -2	40 -67 -77 165 170 162 162 162	$\begin{array}{r} 61\\ 57\\ 56\\ 54\\ 54\\ 49\\ 40\\ 40\\ 40\\ 32\\ 35\\ 30\\ 30\\ 30\\ 33\\ 30\\ 33\\ 4\\ 30\\ 33\\ 4\\ 30\\ 22\\ 22\\ 22\\ 22\\ 22\\ 22\\ 22\\ 22\\ 22\\ 2$
34	-2	162	-34

35	7	167	-37
36	-2	161	-33
37	12	165 170	-44
38	17	170	-47
39	-4	164	-33
40	-3	164	
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42	-3	164	-32
43	4	167	-34
44	2	163	-37
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46 47	-2	165	-32
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51 52 53	8	168	-35
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62 63 64	0	167	-33
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64	9	170	-35
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68	16	180	-57
69	20	172	-39

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72	2	168	-34
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75	15	172	-42
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90	13	169	-49
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92	11	170	-48 -47
93	11	170	-47
94	16	171	-49
95 96 97	15	171	-48
96	12 27	170	-48
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101	26	171	-62
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108 109	26	172	-5
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111 112	25 35	172	-5
143	30	172	-5
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117 118	65	174	-9
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123 124	<u>68</u> 95	173	-9
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65 66	278	154	-28 -27
67	268	155	-27
68 69	267	156	-26
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74 75	315 312	149	
76	309	149	-30 -29
77	308	150	-29
78 79	294 333	139	-28
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81 82	394 360	155	-33
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07 08	398 403	142	-35: -36
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227	486	142	-40
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252	513	132	-42
253	531	125	-44
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196	475	21	-259 -265
598	473	33	-268
199 100	550 569	<u> </u>	-323 -311
101	532	-6	-302
102	522	-3	-297
103 104	<u>515</u> 509	<u>0</u> 3	-293 -290
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06	502 499	7 8	-286
107	499	18	-284 -280
09	556	-1	-329
10	561 526	10	-308 -299
12	521	-5	-295
13	537	-2	-311
14	540	-7	-317 -311
16	521	-10	-298
17	511 503	-8 -5	-290 -285
19	497	-4	-281
20	492	-2	-278
21 22	487	-1	-274 -272
23	513	25	-279
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28 29	530 514	-11	-303
30	499	-11 -11	-279
31	491	-9	-275
32 33	486 480	-7 -5	-271
34	475	-3	-265
35	472	-2	-263
36	472 463	2	-261 -253
37 38 39	462 460	1 9	-255

441	464	6	-255
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563	70	122	-69
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568	71	122	-66
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570	74	121	-72
571	73	118	-67
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599	57	135	-40
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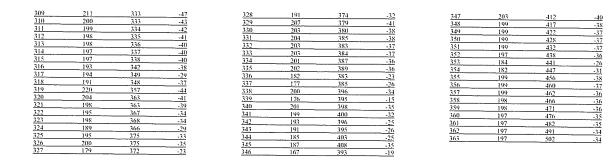
9.5 Complete Raw Data for Cadaver 4

9.5.1 Mid-Palatal Suture Sensor

time	<u>l</u>	2	3
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3	8		4
4	6	7 4	3
5	13	5	
6 7 8 9	5	-0	1
8	6	-5	8 7 6 6
9	6	-4	6
10	5	-13	6
11	6	-13	8
12	8	-12	8
12 13 14 15	<u>8</u>	-14 -16	88 88 99 88 88 88 88 88 88 88 88 88 88 8
15	9	-18	
16	0	-30	9
17 18 19 20 21 22 23 24 25 26 27 20	12	-24	8
18		-38	7
20	7 9	-34 -39	8
20	LI	-34	
22	14	-40	
23	0	-29	1
24	9 10	-12	13
25	10	7 29 45	13
26	9 []	29	1
28	10	57	1
28 29	10	63	1
30	9	72	1
31	11	63 72 72 72 73	1
32 33 34 35 36 37	<u> </u>	73	1
33 34	11	69	1
35	11	<u>66</u> 58	12
36	11	58 51 45 38 33 35 37 84 94 108 118 121 132 137 141 143 142 143 143 143 143 144 143 144 143 144 143 144 143 144 143 144 143 144 147 148 147 149 153 156 164 170 178 180 176 180 176	1'
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38 39	12 12 11	38	
39	11	33	1:
40	0	35	1:
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43	16	78	15
44	13	84	15
45	13	94	9 14 18 15 15 14
46	16 13 13 14 14 14 14 15 15 15 15 15 15 15 15 15 15 15 15 15	108]4
45 46 47 48	14	118	15 16 15
48 49	14	121	16
50	14	137	16
50 51 52	15	141	16
52	15	143	16
53	15	142	16 18 16
54	15	142	10
55 56	15	14.5	16
56 57	15	140	17
58	15	143	17 17 17 18 18 18 18 18 18 18 18
50	16	142	17
50 51 52 53	16	147	
	16	149	18
32	16	153	
1 <u>5</u> 54	16 16	130	18
55	16	170	18
56	16	175	18
56 57 58 59	16 17 17 17 17 17 17 17	178	18
<u>8</u>	17	182	18
59 70	17	181	19 19 19
70	17	176	19
12	17	180	19
2 3 4 5 6	18	178	19
4	18	172	19
5	18	167	20
7	18	164	20
8	19	164	20
19	18	148	20
0	19	144	20
1	19	147	20
2	13	139	19
13 14	-12	127	19 27
5	17	140	2/
6	20	161	20 21
7	13	149	17
8	16	141	19
9	20	133	25
0	20	124	21
2	5	98	24
3	23	98 91	15
4	18	84	21
5	11	74	20
6	22	74	20
7	34	77	11
<u>8</u> 9	29	59	16
9 00	12	-25 -91	17
	66		20
01	8	+142	21

103 104	<u>30</u> 26	-217 -237	<u>10</u> 17
105	21	-245	19
106 107	30	-271	16
108	29	-238	14
109 110	30	-196 -180	15
111	30	-177	<u>16</u> 16
112	21	-178	20
113	47	-158 -143	7 8
115	33	-130	10
116 117	32 35	-126	15
117	36	-114 -120	14
119	38	-113	14
120 121	36	-116 -131	<u>19</u> 4
122	43	-134	8
123 124	32	-151 -192	9
125	44 47	-218	0
125 126	44	-218 -234 -234 -234 -243	9
127	58	-234	<u>6</u> -2
127 128 129 130		-240	0
130 131	46	-233	3
132	<u>63</u> 54	-230 -215	-7 -5
133	41	-205	4
134 135	<u>60</u> 58	-196 -201	<u>-5</u> -10
136	56	-198	-4
137	50	-192	-2
138 139	113	-161 -147	-24
140	95	-138	
141	99 81	-133	-9
142 143	98	-101	
144	80	-97	-1
145 146	94 74	-85	- <u>-5</u> 12
146 147	71	-82 -70	7
148 149	75	-70	<u>9</u> -22
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151 152	105	-36	-8
152	105	-27 -23	-8
154	92	-17	1
<u>155</u> 156	112	-26 -32	-18
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158	96	-25	-5
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161	111	-33	-19
162 163	117	-36 -49	-15
164	119	-63	-11
165	114	-55	-20
166 167	113	-54 -52	<u>-15</u> -24
168	120	-47	-24
169 170	113	-42 -60	-10
171	122	-49	- <u>33</u> -27
172 173	121	-43	-21
173	121	-37 -33	-21
175	121	-24	-18
176 177	117	-32 -27	-10
178	124	-27 -19	-28
179	124	-8	-25
180 181	124 124	4	-24
182	124	18	-22
183 184	123	24	-13
185	125	33	-29
186		39	-26
187 188	133	43	-34 -31
189	127	58	-27
190 191	132	<u>67</u> 76	-28 -27
192	132	86	-27
193	133	94	-26
194 195	132 129	101 105	-25 -23
196	131	115	-24
197	141	114	-33
	1.30	121	-23
198 199	125	131	-1/
198 199 200	125	124	-17
198 199 200 201	120	124 127	<u>.9</u> -34
198 199 200 201 202 203	120 138 141 139	124 127 130 132	-9 -34 -33 -30
198 199 200 201 202	120 138 141	124 127 130	<u>-9</u> -34 -33

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207	142	141	-37
208	133	148	-32 -27 -37 -35
209	145	142	-37
210	152	153	-35
211	141	150	-30
212 213	143	150 155	-27
21.5	162	155	-41 -33
215	140	159	-26
216	151	166	-31
217 218	158	162	-36
218	159	163	-40
219	175	163	-44
220	171	172	-40
221	160	170	-32
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223	166	178	-35
224	166	171	-34
225	163	184	-25
226	162	183	-26
227	159	182	-22
228 229	165	178	-27
230	166	192	-29 -30
231	164	190	.20
232	160	189	-22
232 233	161	191	-28
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241	143	189	-18
242 243	144	190	-17
243	147	193	-22 -20
245	151 151	194	-22
246	141	196	-16
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251	176	219 221 223 227	-33
252	174	221	-32
253	173	223	-32
254	173	227	-31
255 256	173	234	
256	172	239	50
258	172	241	-30 -30 -29
259	171	251	-28
260	171	256	+28
261	171	257	-27
262	171	260	-27
263	180	253	-34
264	179	260	-35
265	157	260	-28
266	146	257	-7
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268	176	276	-33
269 270	177	281	-33
270	174	285	-24
271	174	283 284	-36
272 273	176	287	-3.5
274	176	287	-33
372	176	293	- <u>33</u> -32
276	177	296	-32
275 276 277 278 279	175	297	-30
278	186	294	-30 -32
	181	300	-36
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281	180	303	-34
282	180	305	-34
283		302	-28
284 285	180	306	-35
285	179	307	-24
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288	183	310	-36
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302 303	200	326 325 332	-39
302		332	-39
302 303 304	200	332 333	-39
302 303 304 305	200 197 194	332	-39



9.5.2 Intermaxillary Suture Sensor

time	1	2	3
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12	3	5	1
11 12 13 14	4 5	4	
15	5	4	1
16	4	3	1
15 16 17 18	4	3	
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<u>19</u> 20	6	4	2
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24	6	4	2
25	8	5	2
25 26 27 28	8	5	2
28	8	10	
29 30	5	11	5
30	<u>J</u> L	44	16
31	<u>6</u> 9	5	3
32 33 34	8	6	3
34		20	14
35 36 37 38	6	3 4	3
37	10	7	
38	10	5	12
<u>39</u> 40	8 9	18	9
41	7	4	
42	9	4	5 5 7
43	10	10	7
44 45	11	<u>6</u> 9	6
46	8	22	15
47	10	5	6
48 49	11	6	<u>6</u> 7 7
50	9	16	
51	7	16	13
52 53	9	5	<u>6</u>
54 55	10	8	7 8
55	8	13	10
<u>56</u> 57	8	16	. 11
58	7	10	9
59	5	14	12
60 61	9 9	8	<u>12</u> 7 10
62	10	14	9
63	5	17	9
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66	8	8	
66 67	8	9	8
68 69	6	13	10
70	8	22 21	11
71	9	15	13
72 73	11	26	14
73 74	9 8	16	12 13 17
75	9	13	15
76 77	10	22	18
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79	12	16	15
80	11	15	15
<u>81</u> 82	12 13 12	16	15
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174	12	71	26
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177	13	<u>70</u> 69	25
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178 179	12	68	23
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182	14	66	20
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187	13	72	
188 189	14	<u>69</u> 70	16
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211	16	170	22 32
211 212 213 214 215	19	161	27
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216 217	13	109	16
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218 219	15 17	165	12
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223	15	129	19
224	15	127	18
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230	15	146	19
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231 232	12	145	<u>16</u> 19
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236	13	126 127	8
236 237	15	136	6
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		116	-1
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247 248 249 250	17 15 16	93 99 93	

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269	12	140	-6
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273	13	163	-3
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287	16	146	-20
288	7	161	-17
289	9	165	-12
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291	18	175	-12
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293	16	154	-21
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311	16	133	-34
312	10	137	-39
313	22	164	-40
314	17	136	-42
315	19	129	-40
316	16	167	
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333	23	125	-48
334	23	117	-48
335	23	128	-49
336	23	134	-49
337	8	138	-47
338	20	159	-45
339	28	168	
340	20	138	-50
341	20	136	-50
342	20	136	-50
343		152	
344	18	166	-46
345	25	173	-47
34.3	<u> </u>	175	-51

346	20	149	-50
347	23	149	-49
348	17	176	-32
349	19	117	-25
350	20	147	-20
351	27	114	-17
352	16	104	-15
353	15	107	-15
354	17	108	-18
355	17	109	-19
356	16	102	-22
357	14	102	-23
358	14	140	-21
359	18	161	-20
360	22	129	-29
361	19	121	-26
362	18	122	-33
363	15	122	-77
364	14	119	-27 -27
365	15	122	-28
366	18	161	-28
367	18	148	-30
368	20	147	-36
369	18	124	-35
370	18	132	-32
371	18	131	-34
372	18	137	-34
373	20	189	-29
374	22	150	-35
375	23	151	-33
376	24	197	-33
377	25	164	-39
378	27	165	-43
379	20	139	-37
380	17	136	-31
381	16	121	-32
382	17	131	-29
383	19	126	-31
384	18	124	-31
385	19	126	-32
386	19	127	-31
387	19	124	-34
388	19	123	-35
389	19	122	-35
390	18	121	-36
191 191 192	18	121	-36 -38

9.6 Journal Manuscript for The Angle Orthodontist

<u>Abstract</u>

Quantification of Forces Dissipated Through Bone When Using Rapid Maxillary Expansion

OBJECTIVE: To quantify the forces dissipated through bone when using rapid maxillary expansion in a cadaveric model.

MATERIAL AND METHODS: Stress-strain gauges were bonded to bone of human adult cadavers adjacent to the mid-palatal and intermaxillary sutures using a cyanoacrylate adhesive. The gauges were used to record the forces exerted on the craniofacial complex using a modified RME. Values generated were converted to force in grams.

RESULTS: Complete activation of the modified RPE appliance yielded a mean maximum force value for the mid-palatal suture of 986.58 grams (± 203.72), while the intermaxillary suture was 759.99 grams (± 143.77). A statistically significant difference in force values between the mid-palatal and intermaxillary sensor sites was found (p<0.05). No specimens were found to have either the mid-palatal or intermaxillary suture become patent following activation. The difference in values at the different anatomic locations could indicate that the force generated by the RME becomes dissipated by the hard and soft tissues in the craniofacial complex and that the further away from the RME, the lower the value. This may further support the theory that piezoelectricity mediates alveolar remodelling by orthopaedic appliances or that cell signalling at the cellular level responds to dissipated forces to trigger the osseous response.

CONCLUSIONS: Forces generated by RME devices were dissipated through the bone at levels that exceed orthopaedic force range. The further from the site of force delivery, the lower the values, suggesting dissipation involves many factors including hard and soft tissue which can absorb forces thereby decreasing their magnitude.

INTRODUCTION:

Rapid maxillary expanders (RMEs) are widely used orthopaedic appliances in orthodontics and have existed for over 100 years¹. Since then, a plethora of orthopaedic devices have been established, all having the goal of modifying or altering growth of the craniofacial complex^{2,3}. These include headgears, functional appliances and RMEs. RMEs work by exerting forces on the teeth and bone that are dissipated throughout the craniofacial complex resulting in anatomical changes involving bone remodelling. Although the literature describes the anatomic areas to which this force is dissipated⁴, no investigation has quantified the force on bone at the applied areas and its dissipation throughout the craniofacial complex.

The evidence in the literature describing the clinical efficacy of orthopaedic appliances is exhaustive. It is believed that exogenous forces produced by these appliances result in sutural bone strain that causes a cellular response in growth⁵ Orthopaedic loading on the dentition results in the transmission of these forces to produce tensile and compressive strain on the facial and cranial sutures that absorb and transmit these forces. Sutures absorb these stresses and their bony edges are displaced, either through tension or compression. This results in modulating sutural growth at the cellular level resulting in overall growth modification⁵. Further, different sutures have different responses to force. This force exerts a strain on the sutures of the craniofacial complex resulting in microscopic changes that over time summate to result in macroscopic effects.

Isaacson and others⁶ used strain gauges cemented to RMEs in patients and found that a single activation of the expansion screw of 0.2mm (one quarter revolution) produced approximately 1.3-4.5 kg (3-10 pounds) of force. The force decayed rapidly initially and

then continued to slowly decrease. Isaacson found that the resistance of the expansion was not from the mid-palatal suture but from the bones that articulated the maxilla because there was not a significant change in the force once the sutures opened. He found that a smaller force was required for younger patients versus older patients due to less resistance to expansion of the palate. In a similar study, Zimring and Isaacson⁷ determined that it was the facial skeleton that was the main resistance to expansion. The maximum loads on patients ranged from 7.5-15.7 kg of force during treatment and these forces gradually dissipated during the six week retention period.

In a photoelastic study of the human skull, Chocanos and Caputo⁴ measured stresses using RME of the Haas, Minne-expander, Hyrax, and quad helix types. Each of the appliances produced different stresses transmitted through the bones of the craniofacial complex and effects on the various sutures. Fixed appliances produced stress that was concentrated in the anterior region of the palate that progressed posteriorly toward the palatine bone. The Haas, Minne-expander, and Hyrax appliances resulted in stresses that were in the orthopedic range. The stress was concentrated in the anterior region of the palate and progressed to the posterior and radiated to areas superiorly along the perpendicular plates of the palatine bone deeper to anatomic structures such as the lacrimal, nasal, and malar bones, the pterygoid plates of the sphenoid, the zygomatic process and the medial wall of the orbit. Interestingly, increased activation decreased retention resulting in less of a stress produced at these areas. Furthermore, with increased activation, the palate began to separate. The appliance was found to primarily affect posterior teeth. In a finite element analysis study, Jafari and others⁸ demonstrated that the pterygoid plates are bent more than 2mm during rapid palatal expansion.

Understanding the complex interplay of sutural growth may be the key to understanding the mechanism of action of orthopaedic loading and elucidating a more ideal force to utilize with orthopaedic appliances. This ideal, is the minimum mechanical force that results in the maximum desirable skeletal modification in the shortest period of time.

The current study quantifies the force and assesses the dissipation of the force exerted by an RME at the intermaxillary and mid-palatal sutures on adult cadavers with stress/strain gauges. This exact magnitude of forces may help in better understanding the mechanisms of how sutural growth is affected.

MATERIALS AND METHODS

A stock alginate tray (Ortho Organizers, U.S.A.) was modified by cutting it into 2 equal halves and joined in the center by a 12mm jack-screw (Forestadent, Pforzheim, Germany) soldered to each half with an anterior and posterior contact point (Figure 1). Permission was obtained from the Head o the Department of Anatomy, Faculty of Medicine to perform this study. Human cadavers were selected from the school's Gross Anatomy Laboratory at random and had at least molars and premolars present to allow for better, natural retention of the fabricated RME appliance. In total, 4 suitable cadavers (2 male and 2 female) were used in the study ranging from 68 to 79 years old (mean of 73 years old). Careful dissection of the cadaver was performed in the palatal and intermaxillary area. In the palatal area, an incision was made through the keratinized gingival tissue of the palate. This incision followed the line of the teeth and/or the residual alveolar ridge from the posterior aspect of the second molar to the midline. A flap was then raised

exposing the underlying bone. For the intermaxillary area, an incision was made to cut the gingival tissue in the maxillary anterior area. This incision followed the line of the maxillary anterior teeth and/or the residual alveolar ridge from the area of the first premolar to the midline. A flap was then raised using to expose the underlying bone. The exposed bone was then cleaned thoroughly with gauze dipped in a 99.9% pure ethanol solution for 5 minutes. Next, dry gauze was used to remove any and all moisture from the respective areas for another 5 minutes. A rosette strain gauge sensor (Figure 2) equipped with 6, 10 foot leads (catalogue number C2A-06-062LR-350 (Intertechnologies), was then cemented to the dried bone using MBond200 (Intertechnologies), a cyanoacrylate bonding adhesive. With firm finger pressure, the sensor was placed in position and held for 1 minute to allow the adhesive to dry and ultimately bond to the bone. For the palatal suture, the sensor was placed 2mm to the right of the mid-palatal suture and midway between the anterior segment and the junction of the palatal process of the maxillary bone/palatine bone. The orientation of the sensor was such that the leads faced posteriorly or towards the cadaver's throat. For the intermaxillary suture, the sensor was placed 2mm to the right of the intermaxillary suture and 5mm gingival to the highest point of bone from the tooth or residual alveolar ridge. The orientation of the sensor was such that the leads faced inferiorly or towards the All leads were then connected to the P3 measuring device cadaver's throat. (Intertechnology, Canada) prior to RME placement. Kerr brown dental compound (GAC Dentsply, USA) was placed in a water bath and heated to 60 °C. The compound was then placed and moulded into the modified RME device and placed immediately into the oral cavity of the cadaver. Once the compound cooled and hardened the RME device was

continually activated every 5-10 seconds until it could not be turned any further, for a total of 48 turns or 12 mm. Results were stored directly on the P3 device on a SD memory card and accessed via personal computer into a spreadsheet format. Data obtained was then put through a complex mathematical macro developed by Intertechnology Canada to convert the µstrain value and incorporate the multi-directional axes of the rosette strain gauge into a useable format (force in grams). A two-tailed, paired Student t-test was used to compare the maximum and minimum force values at the different sites for statistical significance between sites and cadavers.

<u>RESULTS</u>

Mid-Palatal Suture Comparisons

There are generally 4 distinct patterns present for each cadaver (Figure 3-6). The first phase can be described as a gradual increase in force values, followed by a second phase involving a more steep or logarithmic increase in force values. The third phase corresponds with a levelling-off followed by the fourth and final phase of a slight decline from the initial levelling-off. Cadaver 4 produced the lowest force values while Cadaver 2, the highest (Table 1). The mean maximum force value obtained for the mid-palatal suture was 986.58 grams (±203.72). Another interesting observation is that Cadavers 2, 3 and 4 (Figure 4, 5, 6) appear to follow the same logarithmic trend in increasing force levels in the second phase of RME activation. Although Cadaver 1 (Figure 3) also shows an increase, it is more gradual as compared to the others. Finally it is apparent that the experiment on Cadaver 1 was the longest test to perform, while Cadaver 4 was the shortest. The display of distinct spikes in the graph occurred at each activation followed

by a period of gradual relaxation and corresponding drop in the force value over time. The spikes that corresponded to activations ranged from 100-300 grams of force.

Intermaxillary Suture Comparisons

The intermaxillary sensor site showed a similar trend as the mid-palatal site, however at different time intervals when compared to the palatal suture site and also lower force values. It is apparent that Cadaver 4 produced the lowest force values while Cadaver 1, the highest (Table 2). The mean maximum force value obtained for the intermaxillary suture site was 759.99 grams (±143.77). Although all cadavers appear distinctly different, it appears that aside from Cadaver 3, the rest appear to follow the same logarithmic trend in increasing force levels in the second phase of RME activation. Finally it is apparent that the Cadaver 1 experiment was the longest test to perform, while Cadaver 4 was the shortest. It is interesting to note that Cadaver 3 (Figure 5) displayed a sudden drop in force values at approximately 451 seconds. The display of distinct spikes in the graph occurred at each activation followed by a period of gradual relaxation and corresponding drop in the force value over time. The spikes that corresponded to activations ranged from 50-350 grams of force.

Maximum force values of all cadavers were compared for statistical significant differences using a two-tailed, paired Student t-test. It was determined that there was a statistical significant difference of the maximum force values between the mid-palatal and intermaxillary sensor site (p<0.05).

DISCUSSION

Despite the extensive research of the effects of the RME appliance, this is the first study that measured the force exerted directly on bone in the human cadaver while activating an RME appliance.

Force values obtained for both the mid-palatal and intermaxillary sites exhibit values that were well within and above the estimated range of orthopaedic values (± 500 grams). Although each cadaver provided specific values and force patterns, there appears to be a general trend of increasing force levels once the RME is activated. There were however detectable differences between cadavers, which are expected due to individual variation from specimen to specimen with varying degrees of bone density soft tissue thickness. Gender may also play a role, as the female cadavers were generally smaller than the male cadavers. Our sample was too small to determine gender differences and as there was no objective way to determine the hard and soft tissue thickness of each cadaver. In Cadaver 3, at approximately 450 seconds, the RME appliance slipped off the Cadaver's oral cavity producing the jump as displayed in Figure 5. In Cadaver 4, some teeth fractured as the expansion was taking place, and as a result, the graph did not follow a gradual increase over time, especially during the first part of the expansion (Figure 6). It is not expected that in a living subject the same type of teeth fracture would occur, due to the elastic fibers in the living subjects, vitality of the PDL and blood supply.

When comparing the 2 sites of sensor placement specifically, it was noted the force levels at the mid-palatal sensor site produced significantly higher values than the intermaxillary

sensor site. Since the force production was further away from the intermaxillary site, this is to be expected. During initial pilot testing, our study involved placement of more sensors at varying sites throughout the craniofacial complex. Those sensors that were placed further away from the RME device registered less force on the P3 measuring device, which confirms the findings of a similar study⁶. This gives credence to the theory that minute orthopaedic forces may have an indirect effect on changes in the craniofacial skeleton via biochemical and/or cellular stimulatory effects induced by dissipated forces. These effects potentially spawned by the dissipated forces and despite being barely measurable, could work at a distance away from the source of the force production.

According to Buckland-Wright⁹, sutures can absorb a considerable amount of energy, which is what probably also occurred in our study. If this were not the case, the force levels would continue to increase with no relaxation or fall in the values as time progressed. Indeed, there were general trends of increases over time, but they levelled off in all of our trials suggesting that not only the sutures, but the surrounding hard and soft tissues may play a role in force dissipation across the craniofacial osseous and non-osseous regions.

All sutures were given a visual and tactile examination following complete activation with no sutures having demonstrated any disconnect from one another, or fracture, despite the 12 mm of activation of the RME appliance. A study by Wehrbein and Yildizhan¹⁰ analyzed the sutures of 18-38 year-old cadavers and found fusion had not actually occurred but the cadavers in our study were much older and cannot be accurately

compared as a result. Wehrbein and Yildizhan also demonstrated that different cadavers exhibited different degrees of suture obliteration. This was confirmed by Persson and Thilander in 1977 who even found a 54 year-old subject without ossification¹¹. Furthermore, even if the mid-palatal suture were to break, it must be borne in mind that in elderly specimens there is additional resistance at the pterygomaxillary interface from the pterygoid plates of the sphenoid bones, which have a tendency to bend laterally and prevent the posterior area of the suture from opening^{4, 8, 12}.

With RME appliances, the opening of the suture generally follows a fan-shape pattern with a larger opening in the anterior area and less in the posterior. This may indicate a higher force value in the anterior area or less resistance to expansion. In the photoelastic study of Chaconas and Caputo⁴, it was found that the stresses generated in the anterior region of the palate were higher and became less and less posteriorly. This was not the case in our study as the forces generated in the anterior area were significantly less than the posterior area (P<0.05). The explanation for this could be that Chaconas's study involved a plastic simulation of a human skull and did not factor in the effect of soft tissue which was taken into account in our study. Anatomy may play a role in the fanshape expansion pattern as there are only soft tissue structures anteriorly and posteriorly more hard tissue structures present which can impede or lessen the effect of expansion. This probably accounts for the higher force generation in the palatal area. However, Chaconas et al⁴ found that the forces generated were in fact orthopaedic in nature which was confirmed in our study. Regardless, it is considered appropriate to generate higher

forces in older patients requiring RME so that the force can be used to achieve some orthopaedic change, as described by Isaacson (1964).

Isaacson et al⁶ using strain gauges in RME's found that large forces of 1.3-4.5 kg were achieved from single activations with rapid initial decay. Zimring and Isaacson⁷ found that these forces were even higher in a subsequent study (7.5-15.7 kg). Although our study did not produce values as high as these, it could be because Isaacson et al put the sensor directly on the RME, whereas our sensor was directly on the bone. This difference can therefore be postulated on the basis of the force which may have been dissipated through all surrounding structures, including hard and soft tissues.

Oberheim and Mao¹³ found that bone strain was higher in younger skulls than in older skulls. Using this study as an example, it would be fair to assume that the forces generated in our study would result in even higher force values in younger patients due to their bone being less stiff than adult bone and subject to greater deformation. However, according to the finite element analysis study of Holberg et al¹⁴, higher cranial base stresses were displayed due to the decrease in elasticity of the adult skull versus the young skull.

Our study also confirmed the findings of Timms'¹⁵ which demonstrated the greatest stress in the area it is being delivered, while further away, it diminishes. In concert with these previous studies, our research confirms the theory of orthopaedic force decay and dissipation along the anatomic structures of the craniofacial complex.

CONCLUSIONS

- Forces generated by RME devices are dissipated through the bone to the midpalatal and intermaxillary sutures at levels that are consistent with the orthopaedic force range.
- Orthopaedic forces generated at both the mid-palatal and intermaxillary sutures do not result in suture patency in aged cadavers.
- The further away from the site of force delivery, the lower the recorded force values, suggesting forces dissipate and diminish as they are transferred along the hard tissue and possibly absorbed by the sutures and surrounding soft tissue.
- Despite the small magnitude of dissipated forces at distant sites, those forces may nevertheless be at levels sufficient to enable a cell signalling response at the cellular level thus generating a histobiochemical reaction and osteogenic response.

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Figure Legends:

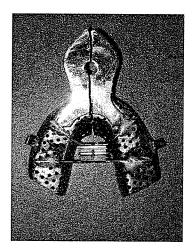


Figure 1: 12mm hyrax expansion screw soldered to a sectioned impression tray

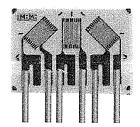


Figure 2: A rosette strain gauge sensor equipped with 6, 10 foot leads (catalogue

number C2A-06-062LR-350 (Intertechnologies))

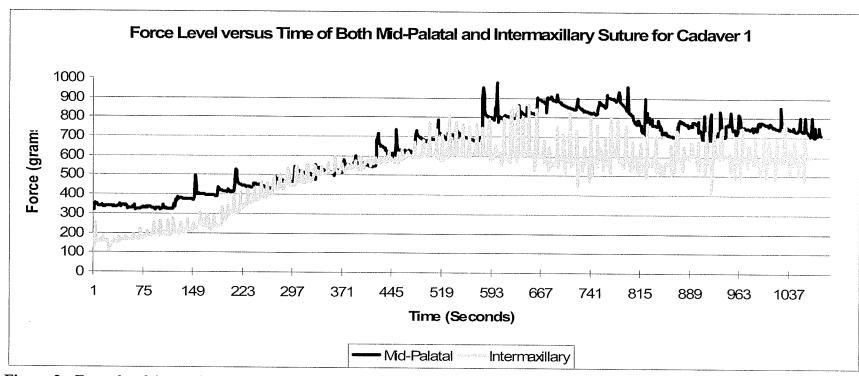


Figure 3: Force level (grams) versus time (seconds) of both mid-palatal and intermaxillary suture for cadaver 1

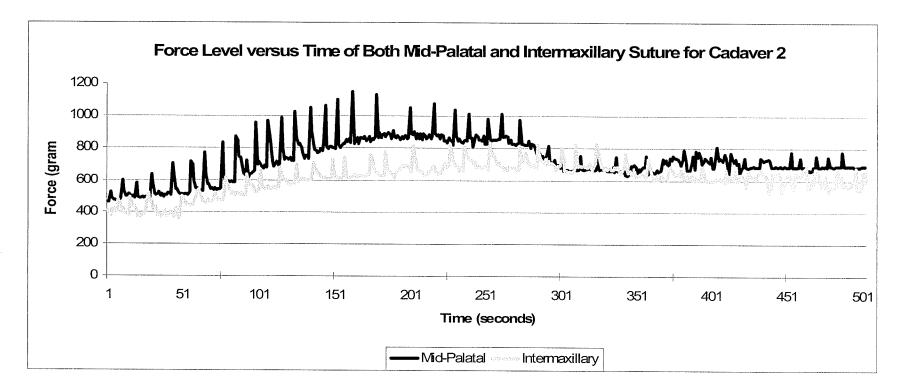


Figure 4: Force level (grams) versus time (seconds) of both mid-palatal and intermaxillary suture for cadaver 2

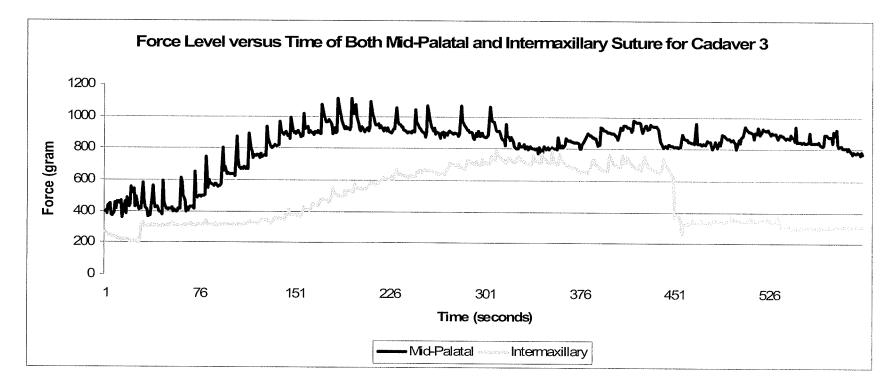


Figure 5: Force level (grams) versus time (seconds) of both mid-palatal and intermaxillary suture for cadaver 3

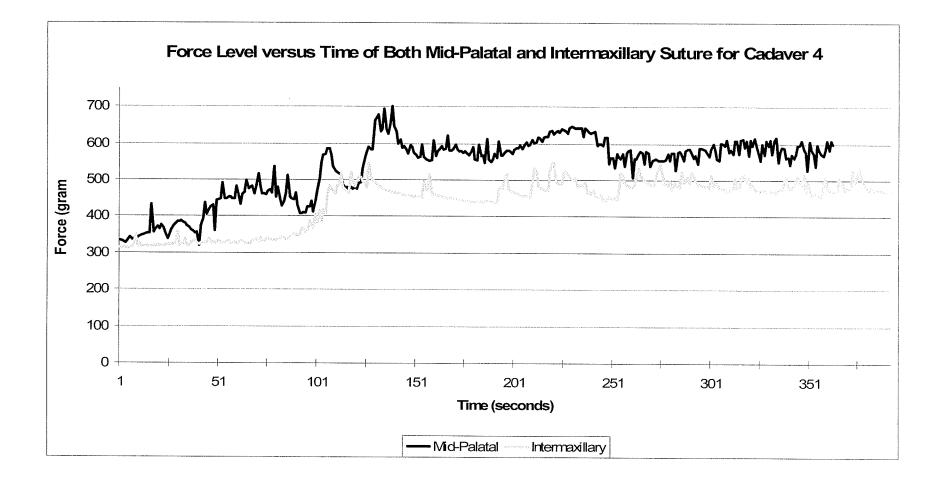


Figure 6: Force level (grams) versus time (seconds) of both mid-palatal and intermaxillary suture for cadaver 4

	Maximum	Minimum	Difference
Cadaver 1	980.27	319.18	661.09
Cadaver 2	1152.42	461.36	691.06
Cadaver 3	1112.05	361.46	750.59
Cadaver 4	701.59	319.44	382.15

Table 1: Maximum and minimum force values (grams) of the mid-palatal sensor

site for all cadavers

	Maximum	Minimum	Difference
Cadaver 1	862.89	111.58	751.31
Cadaver 2	835.84	357.22	478.62
Cadaver 3	792.49	199.55	592.94
Cadaver 4	548.77	312.63	236.14

Table 2: Maximum and minimum force values (grams) of the intermaxillary sensor

site for all cadavers